



## INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

<b>(51) International Patent Classification <sup>6</sup> :</b> <b>A61K 9/20, 9/50, 31/00</b>	<b>A1</b>	<b>(11) International Publication Number:</b> <b>WO 99/12524</b> <b>(43) International Publication Date:</b> 18 March 1999 (18.03.99)
<b>(21) International Application Number:</b> PCT/DK98/00388 <b>(22) International Filing Date:</b> 10 September 1998 (10.09.98)  <b>(30) Priority Data:</b> 1044/97 11 September 1997 (11.09.97) DK  <b>(71) Applicant (for all designated States except US):</b> NYCOMED DANMARK A/S [DK/DK]; Langebjerg 1, Postboks 88, DK-4000 Roskilde (DK).  <b>(72) Inventors; and</b> <b>(75) Inventors/Applicants (for US only):</b> SKINHØJ, Annette [DK/DK]; Moseholmene 3B, DK-2610 Rødovre (DK). BERTELSEN, Poul [DK/DK]; Duevej 42, 4. th., DK-2000 Frederiksberg (DK).  <b>(74) Agent:</b> PLOUGMANN, VINGTOFT & PARTNERS A/S; Sankt Annæ Plads 11, Postboks 3007, DK-1021 København (DK).		<b>(81) Designated States:</b> AL, AM, AT, AT (Utility model), AU, AZ, BA, BB, BG, BR, BY, CA, CH, CN, CU, CZ, CZ (Utility model), DE, DE (Utility model), DK, DK (Utility model), EE, EE (Utility model), ES, FI, FI (Utility model), GB, GE, GH, GM, HR, HU, ID, IL, IS, JP, KE, KG, KP, KR, KZ, LC, LK, LR, LS, LT, LU, LV, MD, MG, MK, MN, MW, MX, NO, NZ, PL, PT, RO, RU, SD, SE, SG, SI, SK, SK (Utility model), SL, TJ, TM, TR, TT, UA, UG, US, UZ, VN, YU, ZW, ARIPO patent (GH, GM, KE, LS, MW, SD, SZ, UG, ZW), Eurasian patent (AM, AZ, BY, KG, KZ, MD, RU, TJ, TM), European patent (AT, BE, CH, CY, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE), OAPI patent (BF, BJ, CF, CG, CI, CM, GA, GN, GW, ML, MR, NE, SN, TD, TG).  <b>Published</b> <i>With international search report.</i>
<b>(54) Title:</b> MODIFIED RELEASE MULTIPLE-UNITS COMPOSITIONS OF NON-STEROID ANTI-INFLAMMATORY DRUG SUBSTANCES (NSAIDs)  <b>(57) Abstract</b>  An oral pharmaceutical modified release multiple-units composition for the administration of a therapeutically and/or prophylactically effective amount of a non-steroid anti-inflammatory drug substance (in the following abbreviated "an NSAID substance") to obtain both a relatively fast or quick onset of the therapeutic effect and the maintenance of a therapeutically active plasma concentration for a relatively long period of time. The modified release multiple-units composition comprises at least two fractions of multiple units such as a first and a second fraction. The first fraction comprises individual units which are designed to quickly release the drug substance and the second fraction comprises individual units which are designed to slowly release the drug substance to enable a delayed and extended release of the drug substance. Typically, the second fraction comprises multiple units which are coated with a sustained release coating designed to release the drug substance in such a manner that the maintenance of a therapeutically active plasma concentration for a relatively long period of time are obtained. By suitable adjustment of the release pattern of the at least first and second fraction a composition is obtained which is adapted to once- or twice-a-day administration.		

**FOR THE PURPOSES OF INFORMATION ONLY**

Codes used to identify States party to the PCT on the front pages of pamphlets publishing international applications under the PCT.

AL	Albania	ES	Spain	LS	Lesotho	SI	Slovenia
AM	Armenia	FI	Finland	LT	Lithuania	SK	Slovakia
AT	Austria	FR	France	LU	Luxembourg	SN	Senegal
AU	Australia	GA	Gabon	LV	Latvia	SZ	Swaziland
AZ	Azerbaijan	GB	United Kingdom	MC	Monaco	TD	Chad
BA	Bosnia and Herzegovina	GE	Georgia	MD	Republic of Moldova	TG	Togo
BB	Barbados	GH	Ghana	MG	Madagascar	TJ	Tajikistan
BE	Belgium	GN	Guinea	MK	The former Yugoslav Republic of Macedonia	TM	Turkmenistan
BF	Burkina Faso	GR	Greece	ML	Mali	TR	Turkey
BG	Bulgaria	HU	Hungary	MN	Mongolia	TT	Trinidad and Tobago
BJ	Benin	IE	Ireland	MR	Mauritania	UA	Ukraine
BR	Brazil	IL	Israel	MW	Malawi	UG	Uganda
BY	Belarus	IS	Iceland	MX	Mexico	US	United States of America
CA	Canada	IT	Italy	NE	Niger	UZ	Uzbekistan
CF	Central African Republic	JP	Japan	NL	Netherlands	VN	Viet Nam
CG	Congo	KE	Kenya	NO	Norway	YU	Yugoslavia
CH	Switzerland	KG	Kyrgyzstan	NZ	New Zealand	ZW	Zimbabwe
CI	Côte d'Ivoire	KP	Democratic People's Republic of Korea	PL	Poland		
CM	Cameroon	KR	Republic of Korea	PT	Portugal		
CN	China	KZ	Kazakhstan	RO	Romania		
CU	Cuba	LC	Saint Lucia	RU	Russian Federation		
CZ	Czech Republic	LI	Liechtenstein	SD	Sudan		
DE	Germany	LK	Sri Lanka	SE	Sweden		
DK	Denmark	LR	Liberia	SG	Singapore		
EE	Estonia						

## **MODIFIED RELEASE MULTIPLE-UNITS COMPOSITIONS OF NON-STEROID ANTI-INFLAMMATORY DRUG SUBSTANCES (NSAIDs)**

The present invention relates to an oral pharmaceutical modified release multiple-units  
5 composition for the administration of a therapeutically and/or prophylactically effective  
amount of a non-steroid anti-inflammatory drug substance (in the following abbreviated  
"an NSAID substance") to obtain both a relatively fast or quick onset of the therapeutic  
effect and the maintenance of a therapeutically active plasma concentration for a  
relatively long period of time. The modified release multiple-units composition comprises  
10 at least two fractions of multiple units such as a first and a second fraction. The first  
fraction comprises individual units which are designed to quickly release the drug  
substance and the second fraction comprises individual units which are designed to  
slowly release the drug substance to enable a delayed and extended release of the drug  
substance. Typically, the second fraction comprises multiple units which are coated  
15 with a sustained release coating designed to release the drug substance in such a  
manner that the maintenance of a therapeutically active plasma concentration for a  
relatively long period of time are obtained. By suitable adjustment of the release pattern  
of the at least first and second fraction a composition is obtained which is adapted to  
once- or twice-a-day administration.

20

### **TECHNICAL BACKGROUND**

Drug levels can be maintained above the lower level of the therapeutic plasma  
concentration for longer periods of time by giving larger doses of conventionally  
25 formulated dosage forms. However, it is not a suitable approach to increase dosage as  
such doses may produce toxic and undesired high drug levels. Alternatively, another  
approach is to administer a drug at certain intervals of time, resulting in oscillating drug  
levels, the so-called peak and valley effect. This approach is generally associated with  
several potential problems, such as a large peak (toxic effect) and valley (non-active  
30 drug level) effect, and a lack of patient compliance leading to drug therapy inefficiency  
or failure. If, however, the plasma concentration is kept constant over the therapeutic  
level using conventional tablets, an unacceptably high daily dosage is required if the  
active substance is not administered very frequently.

Controlled release compositions are known which are designed to rapidly release a fraction of a total drug dose. This loading dose is an amount of a drug which will provide a desired pharmacological response as fast as possible according to the biopharmaceutical properties of the drug substance. Generally, such compositions in  
5 some more or less sophisticated manner are composed of a sustained release part and a part which either contains a free amount of the drug substance or it releases the drug substance in the same manner as if the drug substance had been formulated as a plain formulation (e.g. in the form of normal tablets or granulates). Such compositions which initially release a burst of a therapeutic agent and then release the agent at an  
10 essentially constant rate are described, e.g., in WO 95/14460 (Euroceltique S.A.) published on 1 June 1995. The composition described therein relates to a sustained release opioid formulation comprising a plurality of substrates comprising the active ingredient in a sustained release matrix or coated with a sustained release coating comprising a retardant material. The sustained release beads are then coated with an  
15 opioid in immediate release form or, in the case the composition is in the form of a gelatine capsule, an amount of free opioid (i.e. the opioid is included as such and has not been processed into a specific formulation e.g. by means of pharmaceutically acceptable excipients) is incorporated into the gelatin capsule via inclusion of a sufficient amount of opioid within the capsule. In a further alternative, the gelatine  
20 capsule itself is coated with an immediate release layer of the opioid.

Generally, the rationale which lies behind the kind of compositions which have been described to enable an immediate release of a drug substance as well as a sustained release of the drug substance is to combine a traditional formulation approach (such as,  
25 e.g., i) plain tablets which have a disintegration time in water of at the most about 15 min for uncoated tablets, cf. Ph. Eur. (the requirements for coated tablets or capsules are at the most 30 min), ii) a traditionally formulated granulate or iii) loose powder of the drug substance itself) with a controlled release approach. By doing so the immediate release part of the composition is intended to release the drug substance in a manner  
30 which corresponds to a plain tablet formulation or the like and the term "immediate" is in such a context intended to denote that the release of the drug substance is faster than the release from a sustained release composition. The immediate release is in no way intended to be faster than that of a traditional or plain composition.

Especially in those cases where the drug substance has a low solubility in an acidic medium having a pH of from about 1 to about 3, i.e. a pH corresponding to the pH in the stomach, the traditional formulation approach will lead to a pharmaceutical composition which has a suitable fast disintegration time but not necessarily a suitable dissolution rate of the drug substance under acidic conditions, i.e. a plain tablet will rapidly disintegrate into granules but the dissolution of the drug substance from the composition and/or the disintegrated composition under acidic conditions may be unsuitable low due to the solubility properties of the drug substance itself. The availability of a drug substance with respect to absorption, i.e. entrance into the circulatory system, is dependant on the presence of the drug substance on dissolved form as it is generally accepted that only dissolved substances are capable of passing the mucous membranes in the gastro-intestinal tract. Therefore, it is important that the dissolution of the drug substance is suitably fast even under acidic conditions in order to enable an initial absorption already from the stomach so that a true fast or immediate therapeutic response is obtainable. Furthermore, if a drug substance – dependant on pH – can exist on un-ionized as well as ionized form (e.g. acetyl salicylic acid which at an acid pH below its  $pK_a$  value predominantly is present on an unloaded, i.e. un-ionized form, whereas at a pH above its  $pK_a$  value predominantly is present on ionized form). For drug substances which are weak acids it is very important to ensure a proper bioavailability of the drug substance already under acidic conditions in order to achieve a true rapid therapeutic effect. However, the various approaches disclosed with respect to achievement of a combination of a rapid and a sustained effect (e.g. in the publications mentioned above) do not seem to take the above-mentioned factors into account and, hence, there is a need for developing compositions which enable a true rapid onset of the therapeutic effect as well as a sustained effect. To this end, we have especially focused on compositions comprising a drug substance suitable for use in situations where a rapid effect is needed but also in situations where an extended effect is desirable in order to develop compositions suitable for administration less frequent than compositions on the market today, more specifically to enable administration on a once or twice daily basis. Examples of suitable drug substances are, e.g., substances which have a pain relief effect. More specifically, interesting drug substances are those belonging to the class of drug substances normally denoted NSAIDs or NSAID substances.

In EP-A-O 438 249A1 (ELAN Corporation P.L.C.) is given another example of a composition which has been designed to release naproxen immediately and sustained. However, as shown in Example 18 herein, the so-called immediate release of naproxen does not take place under acidic conditions, i.e. conditions prevailing in the stomach.

5 Accordingly, such a composition is not within the scope of the present application.

As will be apparent from the following the present inventors have developed a composition in multiple-units form for a quick release as well and an delayed and extended release.

10

Multiple-units formulation techniques according to the invention aim at a modified release of a drug substance in a predetermined pattern to control the peak plasma concentration without affecting the bioavailability, i.e. the extent of drug availability. The release of an NSAID substance from a composition according to the present invention is  
15 controlled in a very flexible manner as described below. Many advantages are obtained, e.g., the frequency of undesirable side effects may be reduced, and due to the control of the time it takes to obtain the peak plasma concentration and the prolongation of the time at the therapeutically active plasma concentration, the frequency of the administration may be reduced to a dosage taken only twice or once a day. This also  
20 serves to improve patient compliance. A further advantage of the modified release multiple-units dosage form is that high local concentrations of the active substance in the gastro-intestinal system are avoided, due to the units being distributed freely throughout the gastrointestinal tract, independent of gastric emptying.

25 Moreover, patients suffering from pain and/or inflammatory conditions and/or related conditions very often require high daily dosages of NSAID substances. If such high dosage of an NSAID substance should be given only once a day, the release from the dosage form must be safe, predictable and reliable. The composition should also be very storage stable because an immediate release due to accidental damaging of e.g. the  
30 coating or capsule of a high dosage form may result in undesired high plasma concentrations, so-called dose dumping, which could cause undesired side effects. Furthermore, from a technical point of view, the release rate and the release pattern of the active drug substance from the composition should not significantly change during the shelf-life of the composition. Even a minor change in the release rate and/or release  
35 pattern may have a significant impact on the *in vivo* performance of the composition.

By use of a coated multiple unit dosage form, the risk of dose dumping due to e.g. rupturing of a coating is reduced because the amount of active ingredient in each coated unit is negligible.

5 The compositions according to the present invention are intended to reduce or essentially eliminate problems identified with other kind of compositions intended for administration once daily. Thus, a major disadvantage of the once-a-day treatment in the art may be a low plasma concentration at the end of the dosing period and thereby the lack of therapeutic response. As the treatment of pain and/or inflammatory conditions  
10 and/or related conditions, is a balance of therapeutic effect on the one hand and the risk of side effects on the other hand, e.g. due to accumulation of drug, the dosage interval is generally calculated so that the drug concentration is substantially decreased at the time of intake of the next dosage. Accordingly, the patient will very often suffer from disease symptoms before the drug concentration subsequent to the next dosage has  
15 reached the therapeutic level. In addition, it should be noted that in the treatment of pain and/or inflammatory conditions and/or related conditions, relatively higher dosages, corresponding to a relatively higher peak concentration, are often needed in case the symptoms break through. Accordingly, a relatively higher initial plasma concentration of an NSAID substance may be necessary compared to the plasma concentration at steady  
20 state.

However, to the best of our knowledge no oral non-steroid anti-inflammatory modified release pharmaceutical composition has been disclosed which at the same time can be produced in an easy, cheap and reliable manner and which provides a suitable profile for  
25 release of active substance (under acidic, neutral and basic conditions) resulting in an extended period of action so that the inflammatory condition is both rapidly alleviated after administration and avoided for a period of about 12 to 24 hours.

Therefore, there is a need for developing a composition comprising a non-steroid anti-  
30 inflammatory drug substance permitting the administration of dosages only once or twice a day in a safe and reliable manner, and which is easy to produce, preferably involving conventional production methods and as few production steps as possible. It is also important that an NSAID composition for daily administration comprises the active ingredient in such a way that the composition has a reliable dissolution rate since a

change in the dissolution pattern of the NSAID substance could be disadvantageous for the patient.

#### **BRIEF DISCLOSURE OF THE INVENTION**

5

The purpose of the present invention is to provide an oral modified release multiple-units composition for administration of a daily dosage of an NSAID substance in a dosage form which only requires administration at the most twice daily, preferably once daily, and which overcomes the drawbacks of hitherto suggested formulations of modified  
10 release compositions containing an NSAID substance in that the dosage form both provides a substantially fast release from a first fraction comprising multiple units and a delayed and extended release from a second fraction of multiple units of the NSAID substance whereby alleviation of symptoms is achieved shortly after administration and is maintained for at least 12 hours, preferably 24 hours after administration.

15

A further aspect of the invention is to provide a process for the preparation of a composition of an oral pharmaceutical modified release multiple-units composition containing an NSAID substance, and in addition, a method for treating patients with a composition according to the invention whereby the interval between each  
20 administration is increased to about 12-24 hours.

Accordingly, the present invention relates to an oral pharmaceutical modified release multiple-units composition in unit dosage form for administration of a therapeutically and/or prophylactically effective amount of a non-steroid anti-inflammatory drug  
25 substance (an NSAID substance), a unit dosage form comprising two NSAID-containing fractions,

i) a first NSAID-containing fraction of multiple-units for quick release of the NSAID substance, and

30

ii) a second NSAID-containing fraction of multiple-units for extended release of the NSAID substance,



the first fraction which – when subjected to dissolution method II as defined herein employing 0.07 N HCl as dissolution medium – releases at least 50% w/w of the NSAID substance present in the fraction within the first 20 min of the test,

- 5 the second fraction being in the form of coated delayed release multiple-units for extended release of the NSAID substance.

The present invention also relates to a composition for the administration of a therapeutically and/or prophylactically effective amount of an NSAID substance to  
10 obtain both a relatively fast onset of the therapeutic effect and the maintenance of a therapeutically active plasma concentration for a relatively long period of time, a unit dosage of the composition comprising at least two fractions as follows:

a first fraction of quick release multiple-units for relatively quick release *in vivo* of an  
15 NSAID substance to obtain a therapeutically and/or prophylactically active plasma concentration within a relatively short period of time, and

a second fraction of coated modified release multiple-units for extended release *in vivo* of an NSAID substance to maintain a therapeutically and/or prophylactically active  
20 plasma concentration in order to enable dosing once or twice daily,

the formulation of the first and the second fractions, with respect to release therefrom and with respect to the ratio between the first and the second fraction in the unit dosage, being adapted so as to obtain:

25

a relative fast *in vitro* release of the NSAID substance from the first fraction of quick release multiple-units, as measured by the dissolution method II as defined herein,

an extended *in vitro* release of the NSAID substance from the second fraction of  
30 extended release multiple-units relative to the *in vitro* release of the first fraction of the NSAID substance, as measured by the dissolution method III as defined herein,

the quick release and the extended *in vitro* release being adapted so that the first fraction is substantially released when the release from the second fraction is initiated  
35 corresponding to at least 50% w/w release of the NSAID substance contained in the

first fraction at the time when at the most about 15% w/w such as, e.g., at the most about 10% w/w or at the most about 5% w/w of the NSAID substance contained in the second fraction is released as measured by the dissolution method III as defined herein.

- 5 It should be noted that the dissolution methods mentioned above and throughout the specification of course may be adjusted to specific drug substances and in some cases replaced with other dissolution methods. However, the requirements claimed herein should still be fulfilled.
- 10 The modified release multiple-units dosage forms of the present invention achieve and maintain therapeutic plasma concentrations for a prolonged period of time. In order to achieve the relatively fast absorption for the first fraction it requires that NSAID substances dissolve in the stomach (cf. the discussion above). Since the solubility of an NSAID substance such as, e.g., lornoxicam is  $< 1 \text{ mg} / 100 \text{ ml}$  in 0.1 N HCl (aqueous
- 15 solution of 0.1 N hydrochloric acid) the present inventors have found that incorporation such an NSAID substance in free form or in the form of a traditional formulation does not give the desired quick release under acidic conditions to enable a fast onset of the therapeutic effect *in vivo*. However, and as it will be discussed in detail below, a quick release of an NSAID substance (which is a weak acid or has a very low solubility under
- 20 acidic conditions) takes place under acidic conditions provided that the drug substance is presented in a formulation wherein specific means has been used in order to manipulate the release rate so that the release becomes much faster than from a traditional composition. Thus, in contrast to the prior art composition in which focus only has been on the extended release rate part of the compositions and on the
- 25 possibility of changing the release from this part, the present inventors have found it necessary to adjust the release rate from both the fast and the slow release part of a composition when the NSAID substance either has a very low solubility in 0.1 N hydrochloric acid or has a  $pK_a$  below about 5.5 such as, e.g., about 4-5. Thus, both the fast release fraction and the delayed release fraction must be manipulated with respect
- 30 to release in order to achieve a suitable overall release rate.

The first fraction of the composition constitutes the quick releasing part of the composition whereas the second fraction of the composition constitutes the delayed and extended release part of the composition. In the first fraction, the release rate is

35 primarily governed by the formulation of the fraction, i.e. the ingredients employed and

the processing of the ingredients to obtain the first fraction (cf. Danish Patent Application filed on 10 September 1998 in the name of Nycomed Danmark). In those cases, where a coating is present on the units of the first fraction, the coating may of course also contribute to the control of the release of the active drug substance from  
5 the first fraction. In the second fraction, the release rate is primarily governed by the constitution and thickness of a controlled release membrane which are applied on pellet cores (also denoted "pellets").

The delayed and extended fraction is based on the application of a release controlling  
10 membrane. The release is being controlled by the membrane which makes the formulation much more robust and easier to manipulate and manufacture. Ideally there is no release controlling effect from the uncoated units of the second fraction, i.e. the uncoated multiple-units of the second fraction do not significantly contribute to any control of the extended release of the active drug substance but the uncoated multiple-  
15 units merely release the active drug substance freely without any significant retardation.

The modified release multiple-units dosage forms of the present invention achieve and maintain therapeutic levels and, at the same time, reduces the risks for any side effect, which are believed to be associated with high blood levels of NSAID substances.  
20 Furthermore, the delayed or extended release properties of the coating applied on the second fraction of the multiple-units dosage forms of the present invention are unaffected by the pH in the gastro-intestinal tract.

The first fraction of the multiple-units dosage form of the invention may also be in the  
25 form of coated multiple-units provided that the release rate of such a fraction is so fast in the dissolution medium employed in dissolution method II described herein that at least 50% w/w of the total dose of the first fraction is released within the first 20 min.

When a coating is present on the multiple-units of the first fraction then it could  
30 advantageous be of the same kind as an outer coating on the multiple-units of the second fraction. The employment of the same kind of coating for each fraction may be performed with substantially identical procedures and materials and the production cost can be kept at a low level.

**DETAILED DISCLOSURE OF THE INVENTION**

Accordingly, the present invention relates to an oral pharmaceutical modified release multiple-units composition in unit dosage form for administration of a therapeutically  
5 and/or prophylactically effective amount of a non-steroid anti-inflammatory drug substance (an NSAID substance), a unit dosage form comprising two NSAID-containing fractions,

i) a first NSAID-containing fraction of multiple-units for quick release of the NSAID  
10 substance, and

ii) a second NSAID-containing fraction of multiple-units for extended release of the NSAID substance,

15 the first fraction which - when subjected to dissolution method II as defined herein employing 0.07 N HCl as dissolution medium - releases at least 50% w/w of the NSAID substance present in the fraction within the first 20 min of the test,

the second fraction being in the form of coated delayed release multiple units for  
20 extended release of the NSAID substance.

As discussed above it is very important to secure that the release pattern of the active drug substance contained in the composition is suitable for a composition for administration once or twice daily. The employment of at least two different fractions of  
25 multiple-units gives very flexible formulation parameters. Thus, it is possible to vary i) the percentage of the total dose of the NSAID substance contained in each fraction and ii) the weight ratio between the different fractions. The system (i.e. formulation concept) is therefore very suitable to not only one specific drug substance but can within certain limits be applied on a class or many classes of active drug substances  
30 once the target release profile has been determined. Of course, a change from one active drug substance to another active drug substance may give rise to certain adjustments of the constitution of the individual fractions to the specific substance. In the following is given a discussion of how to determine a target profile for an active drug substance and the release requirements generally applicable for the group of active  
35 drug substances belonging to the non-steroid anti-inflammatory drug substances.

### Dissolution requirements

As described in the following, a target release profile can be designed for any NSAID substance. In the following the target release profile for a selected NSAID substance is described, namely lornoxicam.

Based on the knowledge of the pharmacokinetics of lornoxicam and a study performed by us employing a plain tablet and a solution (Hitzenberger G, Radhofer-Welte S, Takacs F, Rosenow D.: Pharmacokinetics of lornoxicam in man, Postgrad. Med. J. 1990, 66, pp S22-S26), a target in vivo profile for a once daily product has been estimated (Figure 1).

The presumptions made in estimating this target profile were:

- i) a double peak and an effective concentration for 24 hours are desired from a therapeutic point of view (i.e. plasma lornoxicam concentrations at 24 hours should be similar to the plasma concentration obtained 8-12 hours after administration of half the dose in the form of a plain tablet),
- ii) that the first fraction of the composition should have an absorption rate similar to or faster than that of plain tablets
- iii) that the peak concentration should not be higher than the peak concentration observed after administration of half the dose in the form of a plain tablet, and
- iv) that the second peak should appear about 5-6 hours after dosing.

A person skilled in the art is capable of determining the actual values with respect to the above-mentioned provisions and based on such values perform any necessary correction to the estimated profile (target profile).

The estimated target plasma profile as well as the profile from plain tablets have been deconvoluted with plasma concentrations from an oral solution to give an estimated *in vivo* dissolution profile (Figure 2). All data were normalised to a dose of 16 mg. In the deconvolution a time interval of 0.5 hours was employed (cf. Langenbucher F., and H.

Möller: Correlation of *in vitro* drug release with *in vivo* response kinetics. Part I: Mathematical treatment of time functions. Pharm. Ind. 1983, 45, pp 623-8 and Langenbucher F. and H. Möller: Correlation of *in vitro* drug release with *in vivo* response kinetics. Part II: Use of function parameters. Pharm. Ind. 1983, 45, pp 629-33).

5

The presumptions in making this deconvolution were that the daily dose of lornoxicam is the same irrespective of whether a once daily composition or a plain tablet or a solution were administered,

- 10 The estimated *in vivo* dissolution profile for a once daily product can be used as the target *in vitro* profile for the combination of a fast or quick release fraction (i.e. the first fraction) and an extended or slow release fraction (i.e. the second fraction, coated pellets). The estimated *in vivo* dissolution profile for the once daily composition can be used as the target *in vitro* profile, when performing the dissolution tests *in vitro* with 15 hour in 0.1 N HCl and then shift to phosphate buffer pH 7.3 or 7.4 (dissolution methods III or IV described herein). This knowledge has been utilized in order to arrive at the dissolution requirements described in the following.

The presumptions made in using the estimated *in vivo* profile as target for *in vitro* profile 20 were:

- i) that a plain tablet will remain in the stomach for about 1 hour before a passage into the intestine takes place (estimated from the difference in  $T_{max}$  between the solution (0.5 hours) and the plain tablet (1.5 hour),
- 25 ii) that the correlation between the *in vitro* dissolution and the *in vivo* dissolution is a 1:1 correlation, and
- iii) that lornoxicam is absorbed through the whole gastrointestinal tract (including colon)
- 30 in order not to loose any amount of active drug substance ready for absorption into the circulatory system.

Before going into detail with respect to the release requirement to the first fraction, the second fraction and the composition in its final form, in the following is given details

with respect to the target release profile for a once daily lornoxicam composition. The target profile has been estimated as described above.

Target release *in vivo* profile (corresponds to target release profile *in vitro* employing 5 dissolution methods III or IV as described herein):

Time (hours)	% w/w released lornoxicam
0.5	21 (range: 10-25%)
1	29 (range: 15-35%)
10 2	37 (range: 25-45%)
3	42 (range: 30-55%)
4	52 (range: 40-65%)
5	62 (range: 45-70%)
6	69 (range: 50-75%)
15 7	75 (range: 55-80%)
8	79 (range: 60-85%)
9	83 (range: 60-90%)
10	86 (range: 60-95%)
12	89 (range: 65-99%)
20 16	94 (range: at least about 85%)
20	97 (range: at least about 90%)
24	100 (range: at least about 90%)

As apparent from the above, the first fraction must release the active drug substance  
 25 very quickly in 0.1 N HCl or in the dissolution medium employed in dissolution method II  
 described herein, i.e. under conditions simulating the conditions in the stomach and  
 under these conditions the second fraction does not release any significant amount of  
 the active drug substance. In this connection it is important to note that even if the  
 second fractions does not release any significant amount of the active substance within  
 30 the first 20 min or 1 hours under acidic conditions, then the controlled release coating is  
 not necessarily designed as an enteric coating, i.e. a coating which is insoluble at acidic  
 pH and soluble at neutral/basic pH. The compositions according to the invention  
 exemplified in the experimental section are examples on compositions wherein the  
 controlled release coating of the second fractions is not an enteric coating. Furthermore,  
 35 application of an enteric coating on e.g. pellets would not lead to an extended release of

an active drug substance. The release will of course be delayed (no release under acidic conditions) but as the pH becomes neutral and alkaline, then the enteric coating dissolves, i.e. there is no membrane left to control the release.

5 Notably, the release of the active drug substance from the first fraction is at least 55% w/w such as, e.g., at least about 60% w/w, at least about 65% w/w, at least about 70% w/w, at least about 75% w/w or at least about 80% w/w of the total NSAID substance present in the first fraction within the first 20 min of the test, i.e. the dissolution method II (pH corresponding to 0.07 N HCl) as defined in the experimental  
10 section.

In one embodiment the composition may comprise modified release multiple units wherein the *in vitro* dissolution characteristics of the first fraction of quick release multiple-units within 0.5 hour provides a release as defined by the dissolution methods II  
15 as described herein of at least about 50% w/w, at least about 60% w/w, at least about 70% w/w, at least about 80% w/w, at least about 85% w/w, at least about 90% w/w or at least about 95% w/w calculated on the total amount of active drug substance contained in the first fraction.

20 In addition, the composition may comprise modified release multiple units wherein the *in vitro* dissolution characteristics of the first fraction of quick release multiple units within 1 hour provides a release as defined by the dissolution methods II described herein of at least about 50% w/w, such as, e.g., at least about 60% w/w, at least about 70% w/w, at least about 80% w/w, at least about 85%, at least about 90% w/w or at least about  
25 95% w/w calculated on the total amount of active drug substance in the first fraction.

As apparent from the discussion above, the overall release characteristics with respect to release of the active drug substance from the final composition are composed of the release characteristics of the first and the second fraction of multiple-units, respectively.  
30 With regard to compositions containing an NSAID substance intended for administration once or twice daily, the present inventors have found that the release characteristics of the second fractions most suitably should have the following order of magnitude provided that the release characteristics of the first fraction are as discussed above.



Accordingly, the *in vitro* dissolution characteristics of the second fraction of extended release multiple units may in one embodiment within 1 hour provide a release as defined by the dissolution method III described herein in the range of 0%- about 30% w/w, such as, e.g., in the range of 0%- about 20% w/w, in the range of 0%-about 10%w/w such as about 5% w/w calculated on the total amount of active drug substance in the second fraction.

Furthermore, the *in vitro* dissolution characteristics of the second fraction of extended release multiple units may within 3 hours provide a release as defined by the dissolution method III described herein in the range of about 10%-70% w/w, such as, e.g., in the range of about 10%-60% w/w, in the range of about 12%-50% w/w, in the range of 14%-45% w/w, in the range of about 15%-30% w/w, in the range of about 15%-20% w/w such as, e.g., about 17% w/w of the NSAID substance.

Within 6 hours, the *in vitro* dissolution characteristics of the second fraction of extended release multiple units may provide a release as defined by the dissolution method III described herein in the range of about 35%-95% w/w, such as, e.g., in the range of about 50%-90% w/w, in the range of about 50%-80% w/w, in the range of 50%-75% w/w, in the range of about 50%-60% w/w, in the range of about 53%-59% w/w such as, e.g. about 56% w/w of the NSAID substance.

In addition, within 9 hours the *in vitro* dissolution characteristics of the second fraction of extended release multiple units may provide a release as defined by the dissolution method III described herein in the range of about 50%-100% w/w, such as, e.g., in the range of about 60%-98% w/w, in the range of about 65%-95% w/w, in the range of about 70%-90% w/w, in the range of about 70%-80% w/w such as, e.g., about 76% w/w of the NSAID substance.

To ensure that the final composition has a proper constitution with respect to the weight amount of first fraction relative to the amount of second fraction, the *in vitro* dissolution characteristics of the first and second fractions are in one embodiment adapted so that the first fraction is substantially released when the release from the second fraction is initiated, corresponding to at least 50% w/w release of the first fraction at the time at the most about 15% w/w such as, e.g., at the most about 10% or at the most about 5% w/w of the second fraction is released, as measured by

the dissolution method III described herein. In addition, the *in vitro* dissolution characteristics of the first and second fractions in the same or a second embodiment as mentioned above are adapted so that the first fraction is substantially released when the release from the second fraction is initiated, corresponding to at least 70% w/w release of the first fraction at the time at the most about 20% w/w such as, e.g., at the most 15% w/w or at the most about 10% w/w of the second fraction is released, as measured by the dissolution method III described herein.

Apart from the requirements to the individual fractions contained in the composition it is of course of utmost importance to ensure that the composition in its final form has *in vitro* dissolution characteristics which give evidence for a suitable *in vivo* behaviour, i.e. a fast onset of the effect together with an extended release of the active drug substance to ensure a therapeutic and/or prophylactic effect upon administration once or twice daily.

15

The two fractions of multiple units may be selected, with respect to the release from each fraction and the ratio between the two fractions, so that the *in vitro* dissolution characteristics of the composition within 1 hour provide a release of the NSAID substance in the first and second fractions in the range of from about 5% w/w to about 50% w/w, such as, e.g., in the range of from about 5% w/w to about 45% w/w, in the range of from about 15% w/w to about 40% w/w, in the range of from about 20% w/w to about 35% w/w such as about 29% w/w, as defined by the dissolution method III described herein.

25 In addition, the two fractions of multiple units may be selected, with respect to the release from each fraction and the ratio between the two fractions, so that the *in vitro* dissolution characteristics of the composition within 3 hours provide a release as defined by the dissolution method III described herein in the range of from about 20% w/w to about 80% w/w, such as, e.g., in the range of from about 25% w/w to about 70% w/w, the range of from about 30% w/w to about 60% w/w, in the range of from 35% w/w to about 55% w/w such as about 42% w/w.

In an additional aspect, the two fractions of multiple units may be selected, with respect to the release from each fraction and the ratio between the two fractions, so that the *in vitro* dissolution characteristics of the composition within 6 hours provide a release as

35

defined by the dissolution method III described herein in the range of from about 40% w/w to about 98% w/w, such as, e.g., in the range of from about 50% w/w to about 95% w/w, in the range of from about 60% w/w to about 90% w/w, in the range of from about 60% w/w to about 85% w/w, in the range of from about 60% to about 5 83% such as about 69-70% w/w.

Furthermore, the two fractions of multiple units may be selected, with respect to the release from each fraction and the ratio between the two fractions, so that the *in vitro* dissolution characteristics of the composition within 9 hours provide a release as 10 defined by the dissolution method III described herein in the range of from about 50% w/w to about 100% w/w, such as, e.g., in the range of from about 60% w/w to about 99% w/w, in the range of from about 70% w/w to about 98% w/w, in the range of from about 70% w/w to about 97% w/w, in the range of from about 75% w/w to about 96% w/w, such as in the range of from about 80% w/w to about 96%, such as 15 about 80-85% w/w.

In a preferred embodiment, the composition fulfils the above criteria with respect to the dissolution characteristics of the composition in the full time span mentioned.

20 The percentage of NSAID substance in the first fraction is in the range of about 5%-50% w/w such as, e.g., in the range of about 10%-45% w/w, in the range of about 15%-45% w/w, in the range of about 20%-40% w/w, in the range of about 25%-40% w/w, in the range of about 25%-35% w/w such as, e.g., about 30% w/w, calculated on the total amount of NSAID substance in the composition.

25

The percentage of NSAID substance in the second fraction is in the range of about 30%-99% w/w such as, e.g. in the range of about 40%-98% w/w, in the range of about 45%-95% w/w, in the range of about 50%-95% w/w, in the range of about 55%-85% w/w, in the range of about 60%-80% w/w, in the range of about 60%-75% 30 w/w, in the range of about 65%-75% w/w such as, e.g., about 70% w/w, calculated on the total amount of NSAID substance in the composition.

In a preferred embodiment, the multiple units of the second and, when appropriate, the first fraction are coated, cross-sectionally substantially homogeneous pellets.

35

It is preferred that the multiple units of the first fraction result in a peak plasma concentration of the NSAID substance which is substantially the same as the peak concentration resulting from the second fraction. As the peak plasma concentration of the second fraction is adapted so that plasma concentration has a prolonged character

5 due to the dissolution characteristics of the fraction described herein, the peak of this second fraction should preferably substantially represent the upper level of the therapeutic plasma concentration. In a preferred embodiment, the plasma concentration level is of such a size that no NSAID substance is in excess.

10 Since the total amount of NSAID substance contained in the first fraction is balanced compared to the total amount of NSAID substance in the composition, a peak plasma concentration of NSAID substance derived from the first fraction which is higher than the peak concentration resulting from the second fraction does not necessarily represent a substantial waste of the NSAID substance.

15 However, unless the patient suffers from heavy breakthrough symptoms wherein a higher plasma concentration than the plasma concentration for maintaining symptom alleviation often seems to be needed, the concentrations obtained from the first fraction should not exceed the peak from the second fraction.

20 Even in the circumstances wherein the peak of the first fraction is preferably higher than the peak from the second fraction, unsuitable high plasma concentrations (within the toxic level) derived from the first fraction may easily be avoided by adjusting the amount of active drug substance contained in the first fraction.

25 In another embodiment, e.g. in the circumstances wherein the patient is well treated by administration once or twice a day with a composition according to the invention, the first fraction may be adapted so that it results in a peak plasma concentration of the NSAID substance which is lower than the peak concentration resulting from the second

30 fraction. This would not necessarily result in breakthrough symptoms as the NSAID substance remaining in the plasma from the previous dosage administered may contribute to maintaining the plasma concentration sufficiently high until the second fraction of the composition is released. In other cases, the daily dosage may be administered at a suitable time of the day when the patient has experienced less need for the

35 NSAID, e.g. before bedtime.

Accordingly, an important aspect of the invention is an embodiment wherein the first fraction results in a therapeutically active plasma concentration of the NSAID substance until the delayed release of an NSAID substance from the second fraction of modified  
5 release multiple units contributes to the maintenance of a therapeutically active plasma concentration of the NSAID substance.

As discussed above, the multiple-units of the first fraction may be in the form of uncoated pellet cores, coated pellet cores, granules, a granulate or small plain tablets  
10 provided that the requirements with respect to release of active drug substance in 0.1 N HCl and under conditions as those described under dissolution method II herein are fulfilled. In those cases, where the first fraction is in the form of coated pellets, the time lag of the release from the second fraction relative to the first fraction may be obtained by a modified release coating of the second fraction which is present in a  
15 range of about 2%-80% such as, e.g., about 2%-70%, about 2-60%, about 3-50%, about 3-40%, about 4-30%, about 5-20% or about 2-5%, relative to the uncoated unit.

It is also preferred that the modified release coating of the fraction(s) is substantially water-insoluble, but water-diffusible and substantially pH-independent which will  
20 facilitate an absorption independent of the presence of food in the stomach.

### Dosage

In general, the dosage of the active drug substance present in a composition according  
25 to the invention depends *inter alia* on the specific drug substance, the age and condition of the patient and of the disease to be treated.

Compositions according to the invention intended for once daily administration will generally contain a daily dose of the active drug substance whereas compositions  
30 according to the invention intended for twice daily administrations will generally contain half the daily dose of the active drug substance. However, the daily dose may be divided into several dosage forms.

In the following is listed the recommended daily doses for selected NSAID substances.

Aceclofenac: 200 mg

Diclofenac: 100 mg

Etodolac: 400 mg

Fenbufen: 900 mg

5 Fenoprofen: 1.5 g

Flurbiprofen: 200 mg

Ibuprofen: 1.6 g

Indometacin: 100 mg

Ketoprofen: 200 mg

10 Meloxicam: 15 mg

Nabumeton: 1 g

Naproxen: 750 mg

Piroxicam: 20 mg

Sulindac: 300 mg

15 Tenoxicam: 20 mg

Tiaprofenic acid: 600 mg

Tolfenamic acid: 400 mg

Tolmetin: 800 mg

- 20 The amount of an NSAID substance of the modified release multiple-units composition according to the invention may be selected so that it corresponds to about 1 mg, 2 mg, 3 mg, 4 mg, 5 mg, 8 mg, 10 mg, 12 mg, 16 mg, 20 mg, 24 mg, 25 mg, 30 mg, 32 mg, 50 mg, 60 mg, 100 mg, 200 mg, 300 mg, 400 mg, 500 mg, 600 mg, 700 mg, 800 mg, 900 mg, 1 g, 1.1 g, 1.2 g, 1.3 g or 1.6 g of NSAID substance which are
- 25 dosages generally known in the art. However, the composition according to the invention preferably comprises an amount of an NSAID substance which is a daily therapeutically effective amount of the NSAID substance.

Generally, with conventional dosage forms such as plain tablets comprising an NSAID

30 substance, it is not always possible to obtain identical release profiles when different dosages are administered together as the load of active ingredient may differ depending on the size of the tablet. The release profile for 100 mg given in a single dosage may thus differ from 100 mg given as 5 dosages comprising 20 mg each. Not even with the commercially available modified release dosage forms, a substantially identical release

35 profile within the different dosages is always observed.

With a composition according to the present invention, it is now possible to administer different dosages with identical release profiles (cf. results reported in the experimental section). For example, if each modified release multiple-units composition according to 5 the invention is prepared with the same type of multiple units of the first and second fractions and in the same ratios, each of the dosage forms may be administered together to obtain any desired total dosage without altering the overall release profile from the total dosage. Accordingly, reliable and predictable plasma concentrations during the complete time span between administration may be obtained independently 10 of the total dosage.

Therefore, a further advantage of the composition according to the invention is that the composition may be produced in different series of dosage forms of e.g. 4 mg, 8 mg, 12 mg, 16 mg, 24 mg, 32 mg etc., each of the series having individual properties 15 resulting from the design of modified release of the first and second fractions as well as from the ratio between the fractions. Any desired total dosage can then be selected from the relevant dosage forms within each of the series.

The preferred dosage form according to the invention is in the form of a capsule, tablet, 20 sachet etc. The size of the dosage form is adapted to the amount of the NSAID substance of the composition.

The above suggested dosage amounts should not be regarded as a limitation of the scope of the invention as it is obvious for the skilled person that any desired amount of 25 the NSAID substance may be applied and is only limited by the size of the composition and the type of the NSAID substance.

The overall goal of the present invention is to provide a composition in unit dosage form for the administration of a therapeutically effective amount of an NSAID substance once 30 a day. However, as some patients may still need to, or prefer to, receive administration twice a day, the invention should not be limited to a once-a-day composition as long as each of the unit dosage forms fulfils the criteria with respect to the dissolution mentioned above.

In a further aspect, the invention relates to a process for the preparation of an oral pharmaceutical modified release composition, the process comprising incorporating into the unit dosage at least two fractions as follows:

5 a first fraction of quick release multiple-units for relatively quick release *in vivo* of an NSAID substance to obtain a therapeutically or prophylactically active plasma concentration within a relatively short period of time, and a second fraction of coated extended release multiple-units for extended release *in vivo* of an NSAID substance to maintain a therapeutically active plasma concentration in order to enable dosing once or  
10 twice daily,

the formulation of the first and the second fractions, with respect to release therefrom and with respect to the ratio between the first and the second fraction in the unit dosage, being adapted so as to obtain:

15

a relative quick *in vitro* release of the NSAID substance from the first fraction of quick release multiple-units, as measured by the dissolution method II defined herein,

an extended *in vitro* release of the NSAID substance from the second fraction of  
20 extended release multiple-units relative to the *in vitro* release of the first fraction of the NSAID substance, as measured by the dissolution method III as defined herein, the quick release and the extended *in vitro* release being adapted so that the first fraction is substantially released when the release from the second fraction is initiated corresponding to at least about 50% w/w release of the NSAID substance contained in  
25 the first fraction at the time when about 5% w/w of the NSAID substance contained in the second fraction is released as measured by the dissolution method III as defined herein.

#### Definitions of selected terms used herein

30

The term "modified release multiple-units composition" used in the present context is defined as the release of the drug differs from that of a traditional composition. The release rate is in other words controlled and it is possible to manipulate the release rate by means of e.g. changing the formulation parameters. The rate is often controlled in  
35 such a manner that the plasma concentration levels are maintained for the longest



possible period above the therapeutic (the therapeutically active) level, but below the toxic level. However, the term "modified" is not restricted to an extended or prolonged effect, the term "modified" may as well cover the situation where the release rate is manipulated in such a manner that a quicker release than normally expected is obtained.

5 Thus, in the present context the terms "quick", "fast" and "enhanced" release as well as "controlled", "delayed", "sustained", "prolonged", "extended" and other synonyms well known to a person skilled in the art are covered by the term "modified".

The term modified release in the present context refers to a composition which can be  
10 coated or uncoated and prepared by using pharmaceutically acceptable excipients and/or specific procedures which separately or together are designed to modify the rate or the place at which the active ingredient or ingredients are released (Ph. Eur. 97).

The term "extended release" in the present context refers to a modified release  
15 composition of which the release of the active ingredient and its subsequent absorption are prolonged in comparison with a conventional non-modified form (Commission of the European Communities).

The terms "quick release", "fast release" or "enhanced release" in the present context  
20 refer to a modified release composition of which the release of the active ingredient and its subsequent absorption are fast. More specifically, the terms "quick release", "fast release" or "enhanced release" mean that for a composition – when subjected to a dissolution method II described herein – at least about 50% w/w of the active substance is dissolved within the first 20 min of the test.

25

The term "fraction" of multiple units in the present context refers to a part of the multiple units of a dosage unit. One fraction will generally differ from another fraction of multiple units of the dosage unit. Even though only two fractions have been defined, it is within the scope of the invention to have more than two fractions in one dosage unit.  
30 Accordingly, the dosage unit according to the invention comprises at least two fractions.

The term "dosage unit" in the present context refers to one single unit, e.g. a capsule, tablet, a sachet or any other relevant dosage form known within the art. A dosage unit

represents a plurality of individual units which in accordance with the general state of the art may be in the form of a capsule, a tablet, a sachet, etc.

The term "bioavailability" designates the rate and extent to which the drug is absorbed  
5 from the modified multiple-units composition.

In the present context the term "therapeutically active plasma concentration which enables dosing once or twice daily" includes the situation wherein the NSAID substance administered has been metabolised to active metabolites resulting in a therapeutic effect  
10 for the stated period. It also includes the situation wherein the NSAID substance administered is present in a peripheral compartment resulting in a therapeutic effect for the stated period.

The terms "NSAIDs" or "NSAID substances" are used herein to designate a group of  
15 drugs that belongs to non-steroid anti-inflammatory drug substances and pharmaceutically acceptable salts, prodrugs and/or complexes thereof as well as mixtures thereof.

The therapeutic classes mentioned herein are in accordance with the ATC (Anatomical  
20 Therapeutic Chemical) classification system.

#### Active drug substances

In the following are given examples of active drug substances which may be  
25 incorporated in a composition according to the invention. A majority of the active drug substances mentioned are weak acids, i.e. substances which have a  $pK_a$  value below about 5.5 such as, e.g., in a range of from about 3.0 to about 5.5 or in a range of from about 4.0 to about 5.0. In this connection it can be mentioned that the  $pK_a$  value for lornoxicam is about 4.7, for naproxen about 4.2, for indometacin about 4.5 and for  
30 acetylsalicylic acid about 3.5. When such substances which have a  $pK_a$  value of between about 3.0 to about 5.5 is employed in the composition, the present inventors have found that the first fraction should be in the form of uncoated multiple-units as the coating or the manufacture of the units to a form suitable for application of a coating seem to have a retarding effect on the release rate of the active drug substance from  
35 the first fraction (see the experimental section). Moreover, active drug substances like

- those mentioned above (i.e. weak acids having a  $pK_a$  value of at the most about 5.5 or about 5.0) generally have a poor solubility in media having a pH below the  $pK_a$  value; as an example the solubility of lornoxicam at a pH corresponding to 0.1 N HCl is less than about 1 mg/100 ml at room temperature and active drug substances like acetylsalicylic acid, indometacin and naproxen are regarded as substances which are practically insoluble in water and 0.1 N HCl at room temperature. From the discussion relating to solubility and availability of the active drug substance in order to get access to the circulatory system it should be appreciated that the release (dissolution) of the active drug substance from the first fraction should be quick under acidic conditions, e.g., in 0.1 N HCl even if the active drug substance has a very low solubility in this medium. First fractions containing such active drug substances are generally not in the form of coated multiple-units in compositions according to the invention (cf. the discussion above).
- However, when the active drug substance incorporated in a composition according to the invention has a  $pK_a$  value of at least about 5.0 such as at least about 5.5 the multiple-units of the invention may as well be in the form of coated multiple-units such as, e.g., coated pellet cores.
- The first fraction is normally uncoated when the NSAID substance has a solubility in 0.1 N hydrochloric acid at room temperature of at the most about 0.5% w/v such as, e.g. at the most about 0.1% w/v, at the most about 0.05% w/v, at the most about 0.03% w/v, at the most about 0.01% w/w, at the most about 0.007% w/v, at the most about 0.005% w/v, at the most about 0.003% w/v, at the most about 0.002% w/v or at the most about 0.001% w/v.

The first fraction may be coated when the NSAID substance has a solubility in 0.1 N hydrochloric acid at room temperature of at least about 0.1% w/v such as e.g. at least about 0.5% w/v or at least about 1% w/v.

Relevant examples of NSAID substances suitable for use in compositions according to the invention are:

- aminoarylcarboxylic acid derivatives like e. g. enfenamic acid, flufenamic acid,  
5      isonixin, meclofenamic acid, mefenamic acid, morniflumate, niflumic acid, and  
        tolfenamic acid,
- arylacetic acid derivatives like e.g. aceclofenac, acemetacin, amfenac, bromfenac,  
        cimmetacin, diclofenac, etodolac, fentiazac, glucametacin, indomethacin,  
10      lonazolac, metiavinic acid, oxametacine, pirazolac, proglumetacin, sulindac,  
        tiaramide, tolmetin, and zomepirac,
- arylcarboxylic acids like e.g. ketorolac and tinoridine,
- arylpropionic acid derivatives like e. g. alminoprofen, bermoprofen, carprofen,  
        dexibuprofen, fenbufen, fenoprofen, flunoxaprofen, flurbiprofen, ibuprofen,  
        ibuproxam, ketoprofen, loxoprofen, naproxen, oxaprozin, pranoprofen, protizinic  
15      acid, and tiaprofenic acid,
- pyrazoles like e.g. epirizole,
- pyrazolones like e.g. benzpiperylon, mofebutazone, oxyphenbutazone,  
        phenylbutazone, and ramifenazone,
- salicylic acid derivatives like e.g. acetaminosalol, acetylsalicylic acid, benorylate,  
20      eterisalate, fendosal, imidazole salicylate, lysine acetylsalicylate, morpholine  
        salicylate, parsalmide, salamidacetic acid and salsalate,
- thiazinecarboxamides like a.o. ampiroxicam, droxicam, lornoxicam, meloxicam,  
        piroxicam, and tenoxicam,
- others like bucillamine, bucolome, bumadizon, diferenpiramide, ditazol,  
25      emorfazone, nabumetone, nimesulide, proquazone and piroxicam (e.g. in the form  
        of a betacyclodextrin complex).

From a market point especially the following NSAIDs are interesting: lornoxicam,  
diclofenac, nimesulide, ibuprofen, piroxicam, piroxicam (betacyclodextrin), naproxen,  
30      ketoprofen, tenoxicam, aceclofenac, indometacin, nabumetone, acemetacin,  
        morniflumate, meloxicam, flurbiprofen, tiaprofenic acid, proglumetacin, mefenamic acid,  
        fenbufen, etodolac, tolfenamic acid, sulindac, phenylbutazone, fenoprofen, tolmetin,  
        acetylsalicylic acid, dexibuprofen and pharmaceutically acceptable salts, complexes  
        and/or prodrugs and mixtures thereof.

Other relevant active drug substances are COX-2 (COX is an abbreviation for cyclooxygenase) inhibitors like e.g. celecoxib and flosulide.

At present, the most preferred drug substance is lornoxicam and pharmaceutically acceptable salts, complexes and prodrugs thereof. Lornoxicam may be present in a composition according to the invention as the sole drug substance or in combination with other drug substances.

The modified release oral dosage form of the present invention preferably includes an NSAID substance as the therapeutically active ingredient in an amount corresponding to from 1 to about 1600 mg of by weight. Alternatively, the dosage form may contain molar equivalent amounts of pharmaceutically acceptable salts thereof. The dosage form contains an appropriate amount to provide a substantially equivalent therapeutic effect.

A composition according to the invention may contain a further active drug substance. Relevant substances in this context are e.g. antidepressants, opioids, prostaglandine analogs (e.g. misoprostol), glucocorticosteroids, cytostatics (e.g. methotrexate), H<sub>2</sub> receptor antagonists (e.g. cimetidine, ranitidine), proton pump inhibitors (e.g. pantoprazole, omeprazole, lansoprazole), antacids, acetaminophen (paracetamol), penicillamine, sulfasalazine and/or auranofin.

The term "antidepressant" used in the present context includes tricyclic antidepressants as well as other antidepressants and mixtures thereof. Pharmaceutically acceptable salts and/or complexes of antidepressant are also within the definition of antidepressant.

Thus, the term "antidepressant" is used here to designate a group of drugs that have, to varying degrees, antidepressive properties and/or suitable properties with respect to alleviation or treatment of neurogenic pain and/or phantom pain. In the present context the term "antidepressant" encompasses drug substances mainly from the therapeutic class NO6 or from the following drug classification: Psychoanaleptics excluding anti-obesity preparations; anti-depressants/thymoanaleptics including substances used in the treatment of endogenous and exogenous depression such as, e.g., imipramine, nortriptyline, amitriptyline, oxipramol and MAO-inhibiting substances; lithium; combinations of drugs with ataractics; psychostimulants including drugs which increase the psychic and physical performance and which have a fatigue depressing, stimulating effect such as, e.g., fentyllines, fencamfamine, methylphenidate, amphetamines;

pyscholeptic-psychoanaleptic combinations; nootropics [which are a class of psychoactive drugs which are claimed to have a selective action on integrative functions of the CNS. Their action is alleged to be particularly associated with intellectual function, learning and memory. Nootropics include preparations containing substances  
5 such as piracetam, pyritinol, pyrisuccideanol maleate, meclofenoxate, cyprodenate and their combinations with other substances, excluding those products with a vasodilatory action (see the therapeutic class C04A). Combinations with cardiac glycosides are classified in the therapeutic class C01A.]; and neurotonics and other miscellaneous products including products which are not classified above such as single or  
10 combination products containing bisibutiamin, deanol and derivatives, GABA, GABOB, N-acetyl asparaginic acid glutaminic acid and salts, kavain, phospholipid, succinodinitrate.

The presently most interesting drug substances belong to the tricyclic antidepressants.  
15 Relevant examples of antidepressants are: tricyclic antidepressants such as, e.g. dibenzazepine derivatives like carpipramine, clomipramine, desipramine, imipramine, imipraminoxide, imipramine pamoate, lofepramine, metapramine, opipramol, quinupramine, trimipramine; dibenzocycloheptene derivatives like amitriptyline, amitriptyline and chlordiazepoxide, amitriptyline and medazepam, amitriptyline and  
20 pridinol, amitriptyline and perphenazine, amitriptylinoxide, butriptyline, cyclobenzaprine, demexiptiline, nortriptyline, nortriptyline and diazepam, nortriptyline and perphenazine, nortriptyline and fluphenazine, nortriptyline and flupentixol, noxiptilin, protriptyline; dibenzoxepine derivatives like doxepin; and other tricyclic anti-depressants like adinazolam, amoxapine, dibenzepin, dimetacrine, dosulepin, dosulepin and diazepam,  
25 dothiepin, fluacizine (fluoracyzine, toracizin), iprindole, maprotiline, melitracen, melitracene and flupentixol, pizotiline, propizepine, and tianeptine; other antidepressants like 5-hydroxytryptophan, ademetionine, amfebutamone, amfebutamone hydrochloride, amineptine, amineptine hydrochloride, amisulpride, fluoxetine hydrochloride, fluoxetine, hypericin, lithium carbonate, sertraline hydrochloride,  
30 sertraline, St John's wort dry extract, trimipramine maleate, citalopram, citalopram hydrobromide, clomipramine chloride, clomipramine hydrochloride, d-phenylalanine, demexiptiline, demexiptiline hydrochloride, dimethacrine tartrate, dothiepin, dothiepin hydrochloride, doxepin, fluphenazine hydrochloride, fluvoxamine, fluvoxamine hydrogen maleate, fluvoxamine maleate, ginkgo biloba, indalpine, isocarboxazide,  
35 johanniskrauttrockenestrakt, 1-tryptophan, lithium citrate, lithium sulfate, lofepramine,

maprotiline, maprotiline hydrochloride, maprotiline mesilate, medifoxamine, metaprimine fumarate, mianserin, moclobemide, nitroxazepine hydrochloride, nomifensine, nomifensine maleate, nomifensin hydrogenmaleat, oxitriptan, paroxetine, paroxetine hydrochloride, phenelzine, phenelzine sulfate, piracetam, pirlindole, pivagabine, prolintane hydrochloride, propizepine hydrochloride, protriptyline hydrochloride, quinupramine, remoxipride hydrochloride, rubidium chloride, setiptiline maleate, tianeptine sodium, trazodone hydrochloride, venlafaxine hydrochloride, maprotiline, toloxatone, tranlycypromine, trazodone, trazodone hydrochloride, viloxazine, viloxazine hydrochloride, zimelidine, zimelidine dihydrochloride.

10

At present, the most interesting drug substances for use in a composition according to the invention are amitriptyline and/or imipramine and pharmaceutically acceptable salts, complexes and prodrugs thereof. Amitriptyline and/or imipramine may be present in a composition according to the present invention either as the sole drug substance or in combination with other drug substances. Amitriptyline is a very interesting drug candidate with respect to preventing and/or treating neurogenic pains and phantom pains.

15

The term "opioid" is used here to designate a group of drugs that are, to varying degrees, opium- or morphine-like in their properties. The term includes natural and synthetic opioids as well as active metabolites such as morphine-6-glucuronide and morphine-3-glucuronide, and mixtures of opioids. Pharmaceutically acceptable salts and/or complexes of opioids are also within the definition of opioids.

20

Further relevant examples of opioids for use in compositions according to the invention include alfentanil, allylprodine, alphaprodine, anileridine, benzylmorphine, bezitramide, buprenorphine butorphanol, clonitazene, codeine, cyclazocine, desomorphine, dextromoramide, dezocine, diampromide, dihydrocodeine, dihydromorphine, dimenoxadol, dimepheptanol, dimethylthiambutene, dioxaphetyl butyrate, dipipanone, eptazocine, ethoheptazine, ethylmethylthiambutene, ethylmorphine, etonitazene, fentanyl, heroin, hydrocondone, hydromorphone, hydroxypethidine, isomethadone, dextropropoxyphene, ketobemidone, levallorphan, levorphanol, levophenacymorphan, lofentanil, meperidine, meptazinol, metazocine, methadone, metopon, morphine, myrophine, nalbuphine, narceine, nicormorphine, norlevorphanol, normethadone, nalorphine, normorphine, norpipanone, opium, oxycodone, oxymorphone, papaveretum,

30

35

pentazocine, phenadoxone, phenomorphan, phenazocine, phenoperidine, piminodine, piritramide, propheptazine, promedol, properidine, propiram, propoxyphene, sufentanil, tilidine, tramadol, salts thereof, mixtures of any of the foregoing, mixed  $\mu$ -agonists/antagonists,  $\mu$ - and/or  $\kappa$ -agonists, combinations of the above, and the like.

5

Within the scope of the invention is of course that more than one active drug substance may be present in a composition, e.g. more than one NSAID substance and/or drug substances within the same or different therapeutic classes. Specific relevant therapeutic classes are M01A (NSAIDs), R05D, N02 (analgesics), N2A (opioids) and

10 N2B (non-narcotic analgesics).

### Dose

In one embodiment of the present invention, the first fraction of multiple units  
15 comprises an amount of an NSAID substance corresponding to from about 50% to about 5% (between 1/2 and 1/20) of the daily dosage. In patients which are satisfactorily treated on 2-3 daily dosages of a conventional non-sustained formulation, the first fraction may in one example contain an amount of the NSAID substance corresponding to 40% of the daily dosage. The second fraction may then contain the  
20 remaining 60% of the daily dosage.

However, a preferred amount of the first fraction may comprise 30% of the daily dosage and the second fraction 70% of the daily dosage.

25 In another embodiment of the present invention, the first fraction of multiple units comprises an amount of an NSAID substance corresponding to the amount of the NSAID substance necessary for obtaining a therapeutic effect upon a first single oral dose of a conventional non-sustained formulation of the NSAID substance.

### 30 Formulation details

#### First fraction

As described above, the formulation of the first fraction depends on the specific active  
35 drug substance to be incorporated. If the solubility at room temperature in 0.1 N HCl is



low and the  $pK_a$  value is below about 5.5. or 5.0, then the first fraction is in the form of uncoated multiple-units. A very suitable formulation of the first fraction has under such conditions been found to be in the form of a granulate wherein special means have been employed in order to ensure a quick release of the poor soluble active drug substance.

- 5 The granulate is typically prepared by wet-granulation (a process well known for a person skilled in the art) employing as little organic solvent as possible in order to reduce any environmental and personal risk. Furthermore, the present inventors have found that incorporation of an antacid-like substance like, e.g., sodium bicarbonate (sodium hydrogencarbonate), magnesium carbonate, magnesium hydroxide, magnesium
- 10 metasilicate aluminate and other alkaline substance, has a pronounced increasing effect on the release rate.

In one embodiment, the individual units of the relatively fast release fraction according to the invention will normally be a granulate having a size (average diameter) of at the

15 most about 250  $\mu\text{m}$  such as, e.g. at the most about 240  $\mu\text{m}$ , at the most about 230  $\mu\text{m}$ , at the most about 220  $\mu\text{m}$ , at the most about 210  $\mu\text{m}$ , at the most about 200  $\mu\text{m}$ , at the most about 190  $\mu\text{m}$ , at the most about 180  $\mu\text{m}$ , at the most about 175  $\mu\text{m}$ , at the most about 150  $\mu\text{m}$ , at the most about 125  $\mu\text{m}$ , at the most about 100  $\mu\text{m}$ , at the most about 90  $\mu\text{m}$  or at the most about 80  $\mu\text{m}$ .

20

As described above, the first fraction may also be in the form of coated multiple-units such as coated pellets provided that the  $pK_a$  of the active drug substance is at least about 5.0 or 5.5. From the experimental section *inter alia* it appears that such coated cores may have the same coating as the coating of the second fraction, but the

25 thickness of the coating differs in such a manner that the coating of the first fraction is much thinner than that of the second fraction. For further details with respect to coating see below.

#### Second fraction

30

The individual units of the extended release fraction according to the invention will normally be pellets or beads having a size (average diameter) of from about 0.1 to 2 mm. The most preferred pellet size is from 0.5 to 0.8 mm. The pellets or beads comprise a combination of active substance, the NSAID substance and excipients.

When the pellets or beads are not coated, the combination of the active substance and the excipients is referred to as a core.

In the present context, the term "cores which are cross-sectionally substantially  
5 homogeneous" designates cores in which the active substance is not confined to an exterior layer on the core body, in other words normally cores which, through the cross-section of the core body, contain substantially the same type of composition comprising minor particles containing active substance, in contrast to the non-pareil type of cores which each consists of an excipient body with active substance applied to its surface.  
10 From this definition, it will be understood that the cores which are cross-sectionally substantially homogeneous will normally consist of a mixture of active substance with excipient(s), this mixture will not necessarily be qualitatively or quantitatively homogeneous through the total cross-sectional area of the core but may show, e.g., a concentration gradient of the NSAID substance or they may consist substantially solely  
15 of NSAID substance. In the following specification and claims, such cores which are cross-sectionally substantially homogeneous will, for the sake of brevity, often simply be designated "cores".

It is contemplated that the core comprising the NSAID substance in a substantially  
20 homogeneous form provides a more reproducible release of the active ingredient than compared to e.g. particles in which the active ingredient forms part of the coating.

It should, however, be understood that the invention is not limited to pellet formulation containing the above-mentioned cores; in principle, the type of cores can be any kind  
25 such as, e.g. matrices, non-pareil cores as well.

It is preferred that the release profile of the core of the individual unit is substantially non-limiting with respect to the desired release of the coated pellet, e.g. that the core itself provides at least about 90% w/w such as, e.g., at least about 95% w/w, at least  
30 about 97% w/w, at least about 98% such as about 100% release within 1 hour, measured in the *in vitro* dissolution test described in the Examples. However, pellet cores showing a slower release of the active substance are still within the scope of the invention.

**Dosage forms**

The oral pharmaceutical modified release multiple-units formulation according to the invention will typically be a capsule containing a multiplicity of the units, typically more  
5 than 100, a sachet containing a multiplicity of the units, typically more than 1000, or a tablet made from a multiplicity of the units, typically more than 100, in such a manner that the tablet will disintegrate substantially immediately upon ingestion in the stomach into a multiplicity of individual units which are distributed freely throughout the gastro-intestinal tract.

10

In the present context the term "once daily"/"once-a-day" is intended to mean that it is only necessary to administer the pharmaceutical formulation once a day in order to obtain a suitable therapeutic and/or prophylactic response; however, any administration may comprise co-administration of more than one dosage unit, such as, e.g., 2-4  
15 dosage units if the amount of active substance required may not be formulated in only one composition unit or if a composition unit of a minor size is preferred.

In agreement with the above-mentioned definition of "once daily"/"once-a-day", "twice daily"/"twice-a-day" is supposed to mean that it is only necessary to administer the  
20 pharmaceutical formulation at the most twice a day in order to obtain a suitable therapeutic and/or prophylactic response in the patient.

Irrespective of the above-mentioned definitions of "once" and "twice" daily, a dosage unit constructed to deliver the active ingredient after only one daily administration is  
25 preferred. However, due to individual circumstances some patients may need a new dosage after e.g. 12 or 18 hours if the patient e.g. has an abnormal absorption or bowel transit time. If the individual has a relatively fast bowel transit time, some of the active ingredient may be excreted before the full dosage is released, or may be released in the colon from which the absorption may be decreased.

30

A multiple unit pharmaceutical composition according to the present invention is preferably formed as a unit dosage form which upon oral administration disintegrates into a multiplicity of individual units. The dosage unit form is preferably a solid dosage unit form such as, e.g., a tablet, a capsule, or a sachet, especially in the form of  
35 capsules.

The actual load of the NSAID substance in a pharmaceutical composition according to the invention, i.e. the concentration in % w/w of the NSAID substance calculated on the total weight of the multiple units, may depend on the particular NSAID substance employed in the formulation. The formulation principle employed in the present invention is very flexible. As an example it can be mentioned that compositions can be designed so that the load of the NSAID substance in the individual multiple units of the two fractions and the content of the two fractions for one dosage unit comprising e.g. 10 mg of NSAID substance is identical with another dosage unit comprising e.g. 100 mg, the release profile for each of the dosages will be identical. Consequently, an individual total dosage can be administered to the patient by combining the relevant dosage units e.g. selected from a series of 4, 8, 12, 16, 24 and 32 mg of the NSAID substance without altering the overall release profile of the total amount of the NSAID substance administered.

15

The compositions mentioned above may be prepared by conventional methods known in the art. The invention also relates to a method for preparing an oral pharmaceutical modified release multiple-units composition.

## 20 Coating

In a further embodiment, the invention relates to a method for preparing an oral pharmaceutical modified release multiple-units formulation in which

- 25 a) individual units containing an active substance are coated with an inner film-coating mixture ("the inner coat") comprising a film-forming substance,
- b) the thus coated units are optionally provided with a first outer film layer comprising e.g. a stabilizing agent ("the middle coat"),
- c) the thus coated units of the second fraction are optionally provided with a second outer film layer comprising a film-forming agent ("the outer coat"),
- 30 d) a mixture of individual units of the first and second fraction are formulated in a dosage form in the desired ratio of the two fractions.

In general, the inner coating is applied in an amount corresponding to 2-20% w/w. The middle coating, if present, is applied in an amount corresponding to about 4% w/w of

the uncoated units and the outer coat is applied in an amount corresponding to about 1-2% w/w of the uncoated units.

The film-forming agent of step c) may be so selected that adhesion between the units is prevented at elevated temperatures, the coated units are then subsequently heated to a temperature above 40 °C, preferably not above 65-75 °C, and thereby a continuous phase is formed in the inner film layer in homogeneous admixture with the film-forming substance. In some cases, this curing process may also take place before the outer coating layer may be applied.

10

The modified release coating is applied on the multiple units from a solution and/or suspension preferably in an aqueous solvent, but an organic coating composition may also be applied.

15 Examples of film-forming agents which are suitable for use in accordance with the present invention are agents selected from the group consisting of cellulose derivatives such as, e.g., ethylcellulose, cellulose acetate, cellulose propionate, cellulose butyrate, cellulose valerate, cellulose acetate propionate; acrylic polymers such as, e.g., poly-methyl methacrylate; vinyl polymers such as, e.g., polyvinyl acetate, polyvinyl formal, 20 polyvinyl butyryl, vinyl chloride-vinyl acetate copolymer, ethylene-vinyl acetate copolymer, vinyl chloride-propylene-vinyl acetate copolymer; silicon polymers such as, e.g., ladder polymer of sesquiphenyl siloxane, and colloidal silica; polycarbonate; polystyrene; polyester; coumarone-indene polymer; polybutadiene; and other high molecular synthetic polymers.

25

In certain preferred embodiments, the acrylic polymer is comprised of one or more ammonio methacrylate copolymers. Ammonio methacrylate copolymers are well known in the art, and are described in NF XVII as fully polymerized copolymers of acrylic and methacrylic acid esters with a low content of quaternary ammonium groups.

30

In one preferred embodiment, the acrylic coating is an acrylic resin lacquer used in the form of an aqueous dispersion, such as that which is commercially available from Rohm Pharma under the tradename Eudragit®. In further preferred embodiments, the acrylic coating comprises a mixture of two acrylic resin lacquers commercially available from

35 Rohm Pharma under the tradenames Eudragit® RL 30 D and Eudragit® RS 30 D, re-

spectively. Eudragit® RL 30 D and Eudragit® RS 30 D are copolymers of acrylic and methacrylic esters with a low content of quaternary ammonium groups, the molar ratio of ammonium groups to the remaining neutral (meth)acrylic esters being 1:20 in Eudragit® RL 30 D and 1:40 in Eudragit® RS 30 D. Eudragit® RL/RS mixtures are  
5 insoluble in water and in digestive fluids. However, coatings formed from the same are swellable and permeable in aqueous solutions and digestive fluids. The Eudragit® RL/RS dispersions may be mixed together in any desired ratio in order to ultimately obtain a modified release formulation having a desirable dissolution profile. The most desirable modified release formulations may be obtained from a retardant coating based on  
10 Eudragit® NE 30D, which is a neutral resin having a molecular weight of 800,000.

The amount of coating applied is adapted so as to obtain a predetermined dissolution characteristic of the fraction of the composition. The percentage by weight of the modified release coating on the individual pellet will, for the fraction providing the  
15 extended duration of effect of the NSAID substance, be at the most about 20% w/w on an average, such as, e.g. about 15% w/w, about 12% w/w, preferably at the most about 10% w/w on an average, more preferred in the range of about 3% to 6 % w/w on an average, based on the weight of the uncoated individual pellet. The amount of coating applied depends on the predetermined dissolution characteristics of the  
20 particular core composition and the desired release profile of the fraction.

However, the amount of coating applied should also be adapted so that there will be no rupturing problems.

25 The coating may be admixed with various excipients such as plasticizers, anti-adhesives such as, e.g., colloidal silicium dioxide, inert fillers, and pigments in a manner known *per se*.

Tackiness of the water-dispersible film-forming substances may be overcome by simply  
30 incorporating an anti-adhesive in the coating. The anti-adhesive is preferably a finely divided, substantially insoluble, pharmaceutically acceptable non-wetting powder having anti-adhesive properties in the coating. Examples of anti-adhesives are metallic stearates such as magnesium stearate or calcium stearate, microcrystalline cellulose, or mineral substances such as calcite, substantially water-insoluble calcium phosphates or substan-  
35 tially water-insoluble calcium sulphates, colloidal silica, titanium dioxide, barium

5 sulphates, hydrogenated aluminium silicates, hydrous aluminium potassium silicates and talc. The preferred anti-adhesive is talc. The anti-adhesive or mixture of anti-adhesives is preferably incorporated in the coating in an amount of about 0.1-70% by weight, in particular about 1-60% by weight, and preferably about 8-50% by weight of the inner film layer. By selecting a small particle size of the talc, a larger surface area is obtained; the consequent higher anti-adhesive effect makes it possible to incorporate smaller amounts of specific anti-adhesives.

10 The individual modified release coated multiple-units may further comprise a middle coating between the "inner coat" and the "outer coat". Such coating may be adapted to stabilize the controlled release coated multiple-units and to prevent undesired changes of the release profile of each coated unit. Accordingly, the middle lacquer or coating may contribute to stability of the release profile of the dosage unit. Accordingly, the multiple units may further comprise an outer film layer.

15

In one aspect, the outer second layer comprises a water-based film-forming agent which prevents adhesion between the units at elevated temperatures and imparts flowability to the units, the water-based film-forming agent being anti-adhesive at temperatures above about 40 °C, especially temperatures above about 50 °C, such as a temperature  
20 between about 60 °C and about 120 °C, and being selected from diffusion coating materials such as ethylcellulose or enteric coating materials such as anionic poly(meth)acrylic acid esters, hydroxypropylmethylcellulosephthalate, cellulose-acetatephthalate, polyvinylacetatephthalate, polyvinylacetatephthalate-crotonic acid copolymerisates, or mixtures thereof, or water-soluble coating materials such as water-  
25 soluble cellulose derivatives, e.g. hydroxypropylcellulose, carboxymethylcellulose, methylcellulose, propylcellulose, hydroxyethylcellulose, carboxyethylcellulose, carboxymethylhydroxyethylcellulose, hydroxymethylcellulose, carboxymethylethylcellulose, methylhydroxypropylcellulose or hydroxypropylmethylcellulose.

30

Examples of plasticizers for use in accordance with the present invention include triacetin, acetylated monoglyceride, rape oil, olive oil, sesame oil, acetyl tributyl citrate, acetyl triethyl citrate, glycerin, sorbitol, diethyloxalate, diethylmalate, diethylmaleate, diethylfumarate, diethylsuccinate, diethylmalonate, dioctylphthalate, dibutylsebacate,  
35 triethylcitrate, tributylcitrate, glyceroltributyrate, polyethyleneglycol, propyleneglycol,

1,2-propyleneglycol, dibutylsebacate, diethylsebacate and mixtures thereof. The plasticizer is normally incorporated in an amount of less than 10% by weight, calculated on the dry matter content of the coating composition.

## 5 Pharmaceutically acceptable excipients

Apart from the active drug substance in the multiple units, the pharmaceutical composition according to the invention may further comprise pharmaceutically acceptable excipients.

10

In the present context, the term "pharmaceutically acceptable excipient" is intended to denote any material which is inert in the sense that it substantially does not have any therapeutic and/or prophylactic effect *per se*. A pharmaceutically acceptable excipient may be added to the active drug substance with the purpose of making it possible to

15 obtain a pharmaceutical formulation which has acceptable technical properties. Although a pharmaceutically acceptable excipient may have some influence on the release of the active drug substance, materials useful for obtaining modified release are not included in this definition.

20 Fillers/diluents/binders may be incorporated such as sucrose, sorbitol, mannitol, lactose (e.g., spray-dried lactose,  $\alpha$ -lactose,  $\beta$ -lactose, Tablettose®, various grades of Pharmatose®, Microtose or Fast-Floc®), microcrystalline cellulose (e.g., various grades of Avicel®, such as Avicel® PH101, Avicel® PH102 or Avicel® PH105, Elcema® P100, Emcocel®, Vivacel®, Ming Tai® and Solka-Floc®), hydroxypropylcellulose,

25 L-hydroxypropylcellulose (low-substituted) (e.g. L-HPC-CH31, L-HPC-LH11, LH 22, LH 21, LH 20, LH 32, LH 31, LH30), dextrans, maltodextrins (e.g. Lodex® 5 and Lodex® 10), starches or modified starches (including potato starch, maize starch and rice starch), sodium chloride, sodium phosphate, calcium phosphate (e.g. basic calcium phosphate, calcium hydrogen phosphate), calcium sulfate, calcium carbonate. In

30 pharmaceutical formulations according to the present invention, especially microcrystalline cellulose, L-hydroxypropylcellulose, dextrans, maltodextrins, starches and modified starches have proved to be well suited.

Disintegrants may be used such as cellulose derivatives, including microcrystalline cellulose, low-substituted hydroxypropyl cellulose (e.g. LH 22, LH 21, LH 20, LH 32, LH 31,

35



LH30); starches, including potato starch; croscarmellose sodium (i.e. cross-linked carboxymethylcellulose sodium salt; e.g. Ac-Di-Sol®); alginic acid or alginates; insoluble polyvinylpyrrolidone (e.g. Polyvidon® CL, Polyvidon® CL-M, Kollidon® CL, Polyplasdone® XL, Polyplasdone® XL-10); sodium carboxymethyl starch (e.g. Primo-  
5 gel® and Explotab®).

Surfactants may be employed such as nonionic (e.g., polysorbate 20, polysorbate 21, polysorbate 40, polysorbate 60, polysorbate 61, polysorbate 65, polysorbate 80, polysorbate 81, polysorbate 85, polysorbate 120, sorbitane monoisostearate,  
10 sorbitanmonolaurate, sorbitan monopalmitate, sorbitan monostearate, sorbitan monooleate, sorbitan sesquioleate, sorbitan tri oleate, glyceryl monooleate and polyvinylalcohol), anionic (e.g., docusate sodium and sodium lauryl sulphate) and cationic (e.g. benzalkonium chloride, benzethonium chloride and cetrimide) or mixtures thereof.

15

Other appropriate pharmaceutically acceptable excipients may include colorants, flavouring agents, and buffering agents.

In the following examples, the invention is further disclosed.

20

#### BRIEF DESCRIPTION OF THE DRAWING

Figure 1 shows a target plasma profile for lornoxicam together with a profile for plain tablets and solutions used to estimate the target profile,

25

figure 2 shows target *in vivo* dissolution profile for lornoxicam once daily and plain tablets,

figure 3 shows dissolution profiles of lornoxicam compositions containing 8 mg of  
30 lornoxicam; further details are given in Examples 14 and 15 herein,

figure 4 shows dissolution profiles of compositions according to Example 15,

figure 5 shows dissolution profiles of compositions according to Example 17.

35

**MATERIALS AND METHODS**

Materials employed in the compositions which were investigated in the course of development of the present invention were as given in the following. In those cases  
 5 where reference is given to an official pharmacopoeia, the reference is to the current edition of the stated pharmacopoeia.

The following abbreviations are used:

- Ph. Eur.: European Pharmacopoeia  
 10 USP/NF: United States Pharmacopoeia National Formulary  
 DLS: Dansk Lægemiddelstandard

	Materials	Quality	Manufacturer
15	Cellulosum microcristallinum (Avicel PH 101)	Ph.Eur.	FMC
	Polysorbate 20	Ph.Eur.	Henkel
	Lactose monohydrate	Ph.Eur.	DMV
	Carmellose sodium (Blanose 7 LFD)	Ph.Eur.	Aqualon
20	Maltodextrin (Glucidex 2)	USPNF	Roquette
	Pregelatinised Starch (Starch 1500)	USPNF	Colorcon
	Hypromellose (Methocel E 5 Premium)	Ph. Eur.	Dow
	Magnesii stearas	Ph.Eur.	Akcros Chemicals
	Talcum	Ph.Eur.	Whittaker, Clark and Daniels
25	Eudragit NE 30 D	Ph.Eur.	Röhm Pharma GmbH
	Croscarmellose sodium (Ac-Di-Sol)	Ph.Eur.	FMC
	Dibasic Calcium Phosphate, Anhydrous (Calcium hydrogen phosphate, mean particle size approx. 30 µm)	USPNF	Kyowa
30	Sodium bicarbonate (sodium hydrogencarbonate, mean particle size approx. 120 µm)	USPNF	Kirsch
	Hydroxypropylcellulose (HPC L fine)	Ph. Eur.	Nippon Soda
	Low-substituted Hydroxy Propyl Cellulose (LH21)	USPNF	Shin-Etsu
35	Ethanol, 96 %	DLS	Danisco

41

Aqua Purificata

Ph. Eur.

Naproxen

Ph. Eur.

Syntex Pharm.

Polyvidone 30

Ph. Eur.

BASF

Isopropanol

Ph. Eur.

Sveda Kemi

5

Whenever relevant, the mean particle size was determined by employment of a Malvern laser particle size analyser.

In the following five different dissolution methods I-V are described. In the table below 10 is given an overview of the important differences between the five methods:

Dissolution method	Dissolution medium	
	pH	volume
15 I	7.4	900 ml
II	0.07 N HCl	900 ml
III	0.1 N HCl/7.3 <sup>a</sup>	750 ml of medium 1 and 250 ml of medium 2
IV	0.1 N HCl/7.4 <sup>b</sup>	750 ml of medium 1; after 1 hour
20		this medium is changed to 900 ml of medium 2
V	7.3	1000 ml

<sup>a</sup> 750 ml 0.1 N HCl is employed in the first 1 hour of the test and then 250 ml of a 25 medium 2 is added leading to a resulting pH of the dissolution medium of 7.3

<sup>b</sup> 750 ml 0.1 N HCl is employed in the first 1 hour of the test and is then replaced by 900 ml of a medium 2 having a pH of 7.4

The various dissolution methods have been employed to show that the method chosen 30 for determining the dissolution profile of various compositions has an influence on the result obtained, i.e. different dissolution profiles are obtained when employing different dissolution methods.

The dissolution methods given below give details partly with respect to the test method 35 and partly with respect to the analysis method. The following methods are directed to

compositions containing lornoxicam as an example of an NSAID substance; however, in the case of compositions containing other drug substances than lornoxicam the test methods and details with respect to procedure and preparation of reagents are the same apart from an adjustment of the analysis method and the drug substance included in the 5 standard solutions to conditions which are suitable for the drug substance in question. A person skilled in the art will have no difficulties in selecting a suitable method of analysis for a specific drug substance.

#### **DISSOLUTION METHOD I**

10 pH 7.4 (lornoxicam)

##### **Test method**

Apparatus: Ph. Eur. Dissolution test for solid dosage forms and USP XXIII <711>  
15 apparatus 2, equipped with Sotax AT7 and Perkin Elmer UV/VIS Spectrometer Lambda 2. The measurement was performed continuously using Perkin-Elmer Dissolution Software for Lambda Series UV/VIS Spectrometers Version 3.0/ JAN 94. The calculations were performed using the same software.

20 Glass fibre filter: Whatman GF/F

Dissolution medium: 900.0 ml dissolution medium pH 7.4

Number of revolutions: 50 rpm

25

Stirrer: Paddle

Temperature of dissolution medium: 37 °C ± 0.5 °C

30 Measuring times: Every 5 minutes after the start of the test (details appear from the following examples)

##### **Analysis method**

35 Detection wavelength:  $\lambda = 378 \text{ nm}$

Measuring equipment: UV/VIS – spectrophotometer, 1 cm cuvette

Preparation of reagents

5

Dissolution medium: An aqueous solution containing 10.1 mg/ml of sodium hydrogenphosphate dihydrate ( $\text{Na}_2\text{HPO}_4 \cdot 2\text{H}_2\text{O}$ ) and 1.6 mg/ml and sodium dihydrogenphosphate monohydrate ( $\text{NaH}_2\text{PO}_4 \cdot \text{H}_2\text{O}$ ); the pH of the dissolution medium is 7.4.

10

Standards

Stock solutions: 2 stock solutions ( $S_1$  and  $S_2$ ) with a concentration of 200  $\mu\text{g/ml}$  lornoxicam are prepared. Lornoxicam is dissolved in solvent for standards given below.

15

Standards: 20.00 ml of each of the stock solutions are added to the reference vessel (cf. below).

Solvent for standards: 1.5% w/w aqueous sodium acetate solution : methanol (1:1 v/v)

20 Test procedure

900 ml of the dissolution medium are filled to each of the vessels (typically three or six vessels for the product and one vessel for reference solution). The medium is heated to  $37^\circ\text{C} \pm 0.5^\circ\text{C}$ . The product to be tested (e.g. a granulate, pellets, a final

25 composition) is placed in the vessels, and the spindle is started. In the last vessel, 20.0

ml of each of the stock solutions are added. The absorbance of the samples and standards is measured at 378 nm with a zero setting towards the dissolution medium.

The percentage dissolved is measured over a suitable time interval.

30

**DISSOLUTION METHOD II**

0.07 HCl (lornoxicam)

Lornoxicam has a very low solubility in 0.1 N HCl *inter alia* in order to show that the  
5 relatively fast release fraction indeed releases lornoxicam at acidic pH (simulating the pH  
conditions in the stomach), dissolution method II is employed.

**Test method**

10 Apparatus: Ph. Eur. Dissolution test for solid dosage forms and USP XXIII <711>  
apparatus 2, equipped with Sotax AT7 and Perkin Elmer UV/VIS Spectrometer Lambda  
2. The measurement was performed continuously using Perkin-Elmer Dissolution  
Software for Lambda Series UV/VIS Spectrometers Version 3.0/ JAN 94. The  
calculations were performed using the same software.

15

Glass fibre filter: Whatman GF/F

Dissolution medium: 900.0 ml dissolution medium

20 Number of revolutions: 50 rpm

Stirrer: Paddle

Temperature of dissolution medium: 37 °C ± 0.5 °C

25

Measuring time: Every 5 minutes after the start of the test (details appear from the  
following examples)

**Analysis method**

30

Detection wavelength:  $\lambda = 378 \text{ nm}$

Measuring equipment: UV/VIS – spectrophotometer, 1 cm cuvette

**Preparation of reagents**

Dissolution medium: Weigh out 50.0 g of sodium chloride and measure out 141.6 ml of concentrated hydrochloric acid. Dissolve the chemical with distilled water and dilute to 5 25 l with distilled water.

**Standards**

Stock solutions: 2 stock solutions ( $S_1$  and  $S_2$ ) with a concentration of 200  $\mu\text{g/ml}$  10 lornoxicam were prepared. Lornoxicam is dissolved in solvent for standards (cf. below).

Standards: 20.00 ml of each of the stock solutions is added to the reference vessel (cf. below).

15 Solvent for standards: 1.5% w/w aqueous sodium acetate solution : methanol (1:1 v/v)

**Test procedure**

900 ml of dissolution medium are filled to each of the vessels (typically three or six 20 vessels for the product and one vessel for reference solution). The medium is heated to 37  $^{\circ}\text{C} \pm 0.5$   $^{\circ}\text{C}$ . The product to be tested (e.g. a granulate, pellets or a final composition) is placed in the vessel. In the last vessel, 20.0 ml of each of the stock solutions are added. The spindle is started, and the absorbance of the samples and standards is measured at 378 nm with zero setting towards the dissolution medium.

25

The percentage dissolved is measured over a suitable time interval.

**DISSOLUTION METHOD III**

0.1 N HCl / pH 7.3 (lornoxicam)

30

This dissolution method includes a change in pH to simulate the *in vivo* situation.

**Test method**

Apparatus: Ph. Eur. Dissolution test for solid dosage forms and USP XXIII <711> apparatus 2, equipped with Sotax AT7 and Perkin Elmer UV/VIS Spectrometer Lambda

- 5 2. The measurement was performed continuously using Perkin-Elmer Dissolution Software for Lambda Series UV/VIS Spectrometers Version 3.0/ JAN 94. The calculations were performed using the same software.

Glass fibre filter: Whatman GF/F

10

Dissolution medium: 750 ml of dissolution medium 1, after 1 hour 250 ml of dissolution medium 2 are added

Number of revolutions: 50 rpm

15

Stirrer: Paddle

Temperature of dissolution medium:  $37\text{ }^{\circ}\text{C} \pm 0.5\text{ }^{\circ}\text{C}$

- 20 Measuring times: Every 5 minutes after the start of the test (details appear from the following examples)

**Analysis method**

- 25 Detection wavelength:  $\lambda = 378\text{ nm}$

Measuring equipment: UV/VIS – spectrophotometer, 1 cm cuvette

- 30 Preparation of reagents

Dissolution media

Dissolution medium 1: 0.1 N HCl



Dissolution medium 2: Weigh out 73,6 g trisodium phosphate, dodecahydrate ( $\text{Na}_3\text{PO}_4 \cdot 12\text{H}_2\text{O}$ ) and measure out 31,8 ml 0,1 N sodium hydroxide. Dissolve the chemicals in distilled water and dilute to 1000,0 ml with distilled water.

## 5 Standards

Stock solutions: 2 stock solutions ( $S_1$  and  $S_2$ ) with a concentration of 200  $\mu\text{g/ml}$  lornoxicam were prepared. Lornoxicam is dissolved in solvent for standards (cf. below).

10 Standards: 20.00 ml of each of the stock solutions are added to the reference vessel (cf. below).

Solvent for standards: 1.5% w/w aqueous sodium acetate solution : methanol (1:1 v/v)

## 15 Test procedure

750 ml of dissolution medium 1 are filled to each of the vessels (typically three or six vessels for the product and one vessel for reference solution). The medium is heated to  $37^\circ\text{C} \pm 0.5^\circ\text{C}$ . The product to be tested (e.g. a granulate, pellets or a final

20 composition) is placed in the vessel. In the last vessel, 20.0 ml of each of the stock solutions are added. The spindle is started. After 1 hour 250 ml of dissolution medium 2 ( $37^\circ\text{C} \pm 0.5^\circ\text{C}$ ) are added.

The absorbance of the samples and standards is measured at 378 nm with zero setting  
25 towards the dissolution medium.

The percentage dissolved is measured over a suitable time interval.

## DISSOLUTION METHOD IV

30 0.1 N HCl / pH 7.4 (lornoxicam)

This dissolution method includes a change in pH to simulate the *in vivo* situation. Furthermore, this dissolution method has been employed in experiments performed in order to clarify whether a pre-treatment of the product in 0.1 N hydrochloric acid has

any influence on the results obtained afterwards in a dissolution medium having a pH of 7.4.

#### Test method

5

Apparatus: Ph. Eur. Dissolution test for solid dosage forms and USP XXIII <711> apparatus 2, equipped with Sotax AT7 and Perkin Elmer UV/VIS Spectrometer Lambda 2. The measurement was performed continuously using Perkin-Elmer Dissolution Software for Lambda Series UV/VIS Spectrometers Version 3.0/ JAN 94. The

10 calculations were performed using the same software.

Glass fibre filter: Whatman GF/F

Dissolution medium: 750 ml of dissolution medium 1, after 1 hour the medium is  
15 changed to 900 ml of dissolution medium 2.

Number of revolutions: 50 rpm

Stirrer: Paddle

20

Temperature of dissolution medium:  $37\text{ }^{\circ}\text{C} \pm 0.5\text{ }^{\circ}\text{C}$

Measuring times: Every 5 minutes after the start of the test (details appear from the following examples)

25

#### Analysis method

Detection wavelength:  $\lambda = 378\text{ nm}$

30 Measuring equipment: UV/VIS – spectrophotometer, 1 cm cuvette

#### Preparation of reagents

Dissolution media:

35 Dissolution medium 1: 0.1 N HCl

Dissolution medium 2: Distilled water containing 10.1 mg/ml of sodium hydrogenphosphate dihydrate ( $\text{Na}_2\text{HPO}_4 \cdot 2\text{H}_2\text{O}$ ) and 1.6 mg/ml of sodium dihydrogenphosphate monohydrate ( $\text{NaH}_2\text{PO}_4 \cdot \text{H}_2\text{O}$ )

## 5 Standards

Stock solutions: 2 stock solutions ( $S_1$  and  $S_2$ ) with a concentration of 200  $\mu\text{g/ml}$  lornoxicam were prepared. Lornoxicam is dissolved in solvent for standards (cf. below).

10 Standards: 20.00 ml of each of the stock solutions is added to the reference vessel (cf. below)

Solvent for standards: 1.5% w/w aqueous sodium acetate solution : methanol (1:1 v/v)

## 15 Test procedure

750 ml of dissolution medium 1 are filled to each of the vessels (typically three or six vessels for the product and one vessel for reference solution). The medium is heated to  $37^\circ\text{C} \pm 0.5^\circ\text{C}$ . The product to be tested (e.g. a granulate, pellets or a final composition) is placed in the vessel. In the last vessel, 20.0 ml of each of the stock solutions are added. The spindle is started. After 1 hour the medium is decanted carefully and the medium is discarded. To the remaining product in the vessel 900 ml of dissolution medium 2 ( $37^\circ\text{C} \pm 0.5^\circ\text{C}$ ) are added. The absorbance of the samples and standards is measured at 378 nm with zero setting towards the dissolution medium employed.

The percentage dissolved is measured over a suitable time interval.

## DISSOLUTION METHOD V

30 pH 7.3 (lornoxicam)

This dissolution method was used to *inter alia* clarify the influence of pH and/or the specific dissolution medium on the release rate and also to clarify, if the results obtained at pH 7.3 - without any pre-treatment in 0.1 N hydrochloric acid - were different from those obtained with pre-treatment in 0.1 N hydrochloric acid.

The buffer capacity of the dissolution medium employed was investigated to ensure a sufficient capacity. pH in the medium was measured before a product was added and after the end of the test. Both measurements revealed the same pH value (7.28), i.e. the buffer capacity is sufficient.

#### Test method

Apparatus: Ph. Eur. Dissolution test for solid dosage forms and USP XXIII <711> apparatus 2, equipped with Sotax AT7 and Perkin Elmer UV/VIS Spectrometer Lambda 2. The measurement was performed continuously using Perkin-Elmer Dissolution Software for Lambda Series UV/VIS Spectrometers Version 3.0/ JAN 94. The calculations were performed using the same software.

15 Glass fibre filter: Whatman GF/F

Dissolution medium: 750 ml of the dissolution medium 1 and 250 ml of dissolution medium 2, the resulting pH is 7.3

20 Number of revolutions: 50 rpm

Stirrer: Paddle

Temperature of dissolution medium:  $37\text{ }^{\circ}\text{C} \pm 0.5\text{ }^{\circ}\text{C}$

25

Measuring times: Every 5 minutes after the start of the test (details appear from the following examples)

Detection wavelength:  $\lambda = 378\text{ nm}$

30

Measuring equipment: UV/VIS – spectrophotometer, 1 cm cuvette

**Preparation of reagents**

Dissolution media:

**5 Dissolution medium 1: 0.1 N HCl**

Dissolution medium 2: Weigh out 73,6 g trisodium phosphate dodecahydrate ( $\text{Na}_3\text{PO}_4 \cdot 12\text{H}_2\text{O}$ ) and measure out 31,8 ml 0,1 N sodium hydroxide. Dissolve the chemicals in distilled water and dilute to 1000,0 ml with distilled water.

10

**Standards**

Stock solutions: 2 stock solutions ( $S_1$  and  $S_2$ ) with a concentration of 200  $\mu\text{g/ml}$  lornoxicam were prepared. Lornoxicam is dissolved in solvent for standards (cf. below).

15

Standards: 20.00 ml of each of the stock solutions is added to the reference vessel (cf. below).

Solvent for standards: 1,5 % sodium acetate solution : methanol (1:1)

20

**Test procedure**

750 ml of the dissolution medium 1 and 250 ml of dissolution medium 2 are filled to each of the vessels (typically three or six vessels for the product and one vessel for reference solution). The medium is heated to  $37\text{ }^\circ\text{C} \pm 0.5\text{ }^\circ\text{C}$ . The product to be tested (e.g. a granulate, pellets or a final composition) is placed in the vessel. In the last vessel, 20.0 ml of each of the stock solutions are added. The spindle is started. The absorbance of the samples and standards is measured at 378 nm with zero setting towards the dissolution medium.

30

The percentage dissolved is measured over a suitable time interval.

Calculation for all methods

Percentage dissolved was calculated with reference to an external standard in the reference vessel.

5

The concentration of the standard in the reference vessel is calculated by the formula below:

$$10 \quad \text{mg lornoxicam per 1000 ml} = \left( \frac{q_1 \cdot 20}{V} + \frac{q_2 \cdot 20}{V} \right) \cdot \frac{1000}{940}$$

Where:

- $q_1$  = amount of standard weighed out for  $S_1$  (mg)  
 15  $q_2$  = amount of standard weighed out for  $S_2$  (mg)  
 20 = added volume of  $S_1$  and  $S_2$  to the reference vessel (ml)  
 $V$  = dilution volume of the standard (ml)  
 940 = volume in the reference vessel after addition of the standards ( $S_1$  and  $S_2$ ) to the vessel (ml)  
 20 1000 = conversion factor to 1000 ml

The content of lornoxicam as percentage dissolved was calculated from the formula below:

25

$$\frac{abs_{sample} \cdot StA \cdot V \cdot 100}{abs_{StA} 1000 \cdot u} \cdot \frac{n}{100}$$

Where

- $abs_{sample}$  = absorbance measured in each vessel containing samples  
 30  $StA$  = mg lornoxicam pr 1000 ml in the vessel containing standard  
 $V$  = volume of the medium (ml)  
 100 = factor converting to percent  
 $abs_{StA}$  = absorbance measured in vessel containing the standard  
 $u$  = declared content (mg)  
 35  $n$  = potency of the standard (%)

100	=	factor converting to percent
1000	=	factor converting the concentration of the standard to mg/ml

The following examples are intended to illustrate specific embodiments of the present  
5 inventions but are not intended in any way to limit the invention.

## EXAMPLES

The following Examples 1 – 8 relate to the preparation of various cores containing  
10 lornoxicam as an example of an NSAID substance. Example 9 relates to the preparation  
of a quick release granulate, Examples 10-17 illustrate *inter alia* the influence of the  
composition of the pellets or the coat on the release rate and Example 18 relates to an  
immediate release composition disclosed in EP-A-O 438 249.

### 15 EXAMPLE 1

#### Preparation of cores containing lornoxicam and coating of the cores with a CR coating

Batch Nos. 04029831 (uncoated pellet cores) and 05029833 (coated pellet cores) were  
20 prepared.

Lornoxicam pellet cores were prepared by manufacturing of pellet cores and subsequent  
coating with an inner and an outer coat.

25 The pellet cores were prepared by the use of an extrusion/spheronization technique.

The ingredients are listed in Table 1. The ingredients I and II were mixed in a beaker by  
stirring, wetted with 150 g water and then mixed to a homogenous mass. The  
ingredients III to VII were filled into a Moulinex laboratory size mixer and mixed for 5  
30 min, whereafter the homogenous mass was added and mixed. The beaker was rinsed  
with the remaining water and added to the mixer.

Table 1

	Ingredients	Amount (g):
5 I	Lornoxicam	54
II	Polysorbate 20	54
III	Cellulose, microcrystalline	102
IV	Lactose	315
V	Carmellose sodium	3
10 VI	Maltodextrin	12
VII	Pregelatinized starch	60
VIII	Purified water	150 + 18

The resulting mass was extruded in a Nica E 140 extruder with a screen size of 0.6  
15 mm. The extrudate was spheronized in a laboratory size spheronizer at a rotation speed  
of 700 rpm for 4 min. The pellet cores thus produced were dried in a laboratory size  
fluid bed dryer with an inlet temperature of approximately 40° C, and the drying process  
was continued until the outlet temperature has reached approximately 30° C. The total  
drying time was approximately 25 min.

20

The dried pellet cores were fractionated in a Retsch sieving apparatus with a lower  
screen of 0.5 mm and an upper screen of 0.8 mm.

The release of lornoxicam from the pellet cores obtained was determined by dissolution  
25 method I (pH 7.4) and is as follows:

Time	Release (%)
10 min.	52.1
1 h	97.6

30

Thus, the release of lornoxicam from the uncoated pellets is rapid and is almost  
accomplished within about 1 hour.

100 g of these pellet cores were coated with an inner coat and an outer coat in a  
35 laboratory size bottom spray fluid bed coater with a spray pressure of 1 bar for both the



inner coat and the outer coat. The temperature of the coating process was maintained at an inlet temperature of approximately 35° C to 40° C.

The composition of the coating is shown in Table 2:

5

Table 2

Ingredient	Amount (g)
10 <i>Inner coat</i>	
Hypromellose (Methocel E prem)	3.25
Magnesium stearate	0.68
Talc	6.07
Eudragit NE 30 D	216
15 Purified water	274
<i>Outer coat</i>	
Hypromellose (Methocel E5 prem)	4.0
Talc	4.0
20 Purified water	96.0

In the coating process the following amount of inner and outer coat was applied. The amount of dry matter applied calculated in percentage of the pellet core weight also appears from the below:

Inner coat: 35.9 g coating solution (corresponding to a dry matter content of approximately 5.5% w/w of the pellet core weight)  
Outer coat: 12.5 g coating solution (corresponding to a dry matter content of approximately 1% w/w of the pellet core weight)

After the application of the coatings, the coated pellet cores were cured at a bed temperature of approximately 70° C for 30 min, whereafter the coated pellet cores were cooled to a bed temperature below 35° C.

35

After the coating, the coated pellet cores are screened through a 1.2 mm screen. Oversized material is discarded.

## EXAMPLE 2

5

**Preparation of pellet cores according to the invention leaving out a surface active substance from the cores**

Batch No. 09029831 (uncoated pellet cores) was prepared.

10

Lornoxicam pellet cores were prepared by using the ingredients listed in Table 3.

Table 3

15	Ingredients	Amount (g)
I	Lornoxicam	27
II	Cellulose,microcrystalline	54
III	Lactosemonohydrate	216
20 IV	Carmellosesodium	3
V	Purified water	84

The pellet cores were prepared by the use of the extrusion/spheronization technique as described in Example 1, wherein the ingredients I to IV were mixed for 5 min in a  
25 Moulinex laboratory size mixer, whereafter the ingredients V was added.

The release of lornoxicam from pellet cores was determined by dissolution method I (pH 7.4) and is as follows:

30 Time	Release (% w/w)
10 min	19.1
1 h	69.8

From the dissolution data given above it is seen that the release is not accomplished after 1 hour and compared with the result obtained with the uncoated pellet cores in Example 1 it seems as if the inclusion of a surface active agent like e.g. polysorbate 20 has a significant influence on the dissolution rate.

5

**EXAMPLE 3**

**Preparation of pellet cores corresponding to the pellets in Example 1 but in a smaller batch size**

10

Batch No. 09029832 (uncoated pellet cores) was prepared.

This Example is intended to illustrate any relevant variation which may turn up as a dependency of the batch size.

15

Lornoxicam pellet cores were prepared as described in Example 1 with the exception that in Example 3, the amounts of the ingredients listed in Table 4 were used.

Table 4

20

	Ingredients	Amount (g)
I	Lornoxicam	27
II	Polysorbate 20	27
III	Cellulose, microcrystalline	51
25 IV	Lactose	157.5
V	Carmellose sodium	1.5
VI	Maltodextrin	6
VII	Pregelatinized starch	30
VIII	Purified water	60 + 15

30

The release of lornoxicam from these pellets cores was determined by dissolution method I (pH 7.4) and is as follows:

Time	Release (% w/w)
10 min	61.2
1 h	98.0

- 5 Thus, the pellet cores prepared have the same dissolution behaviour as the pellet cores prepared in Example 1, i.e. the batch size seems to be without any significant influence on the release rate.

#### EXAMPLE 4

10

**Preparation of coated pellet cores having a thinner inner coating than the coated pellet cores of Example 1**

Batches Nos. 11029831 (uncoated pellet cores) and 20029832 (coated pellet cores)  
15 were prepared.

Lornoxicam pellet cores were prepared as described in Example 1 with the exception that in Example 4, the amounts of the ingredients listed in Table 5 were used.

20 Table 5

	Ingredients	Amount (g)
I	Lornoxicam	27
II	Polysorbate 20	27
25 III	Cellulose, microcrystalline	51
IV	Lactose	157.5
V	Carmellose sodium	1.5
VI	Maltodextrin	6
VII	Pregelatinized starch	30
30 VIII	Purified water	51 + 15

The release of lornoxicam from these pellets cores was determined by dissolution method I (pH 7.4) and is as follows:

Time	Release (% w/w)
------	-----------------

10 min	63.8
--------	------

1h	100.7
----	-------

5

Accordingly, the release of lornoxicam from the pellet cores is accomplished within 1 hour.

The pellet cores were coated as described in Example 1 with the exception that in  
10 Example 4, 100 g pellet cores were coated with an amount of inner and outer coat as follows:

Inner coat: 20.0 g coating solution (corresponding to a dry matter content of approximately 3% w/w of the pellet core weight).

15 Outer coat: 12.5 g coating solution (corresponding to a dry matter content of approximately 1% w/w of the pellet core weight).

As appears from the above, the amount of dry matter of the inner coat is smaller than in Example 1, whereas the amount of dry matter of the outer coat is the same as in  
20 Example 1. Accordingly, it is expected that the release of lornoxicam from the coated pellets of Example 4 is faster than that of lornoxicam from the coated pellets of Example 1.

#### EXAMPLE 5

25

**Preparation of pellet cores corresponding to those of Example 3 with the exception that the surface active agent is replaced by lactose**

Batch No. 11029834 (uncoated pellet cores) was prepared.

30

Lornoxicam pellet cores were prepared as described in Example 2 with the exception that in Example 5, the ingredients listed in Table 6 were used. Compared with the above Example 3 it is seen that the composition of pellet cores of Example 5 is very similar to those of Example 3, the only differences are that in the pellet cores of Example 3 a

surface active agent (polysorbate 20) is included and the amount of water employed differs a little.

Table 6

5

	Ingredients	Amount (g)
I	Lornoxicam	27
II	Cellulose, microcrystalline	51
10 III	Lactose	184.5
IV	Carmellose sodium	1.5
V	Maltodextrin	6.0
VI	Pregelatinized starch	30.0
VII	Purified water	84.0

15

The release of lornoxicam from these pellets cores were determined by dissolution method I (pH 7.4) and is as follows:

	Time	Release (% w/w)
20	10 min	20.5
	1h	62.4

In conclusion the same pattern is observed as in Example 2, namely that the exclusion of a surface active agent has a decreasing effect on the release rate of lornoxicam from the pellet cores.

## EXAMPLE 6

Preparation of pellet cores having a content of a disintegrant

30

Batch No. 19029834 (uncoated pellet cores) was prepared.

Lornoxicam pellet cores were prepared by using the extrusion/spheronization technique as described in Example 1. However, the ingredients used in Example 6 are listed in

35 Table 7:

Table 7

	Ingredients	Amount (g)
I	Lornoxicam	27
5 II	Polysorbate 20	27
III	Cellulose, microcrystalline	51
IV	Lactose	142.5
V	Carmellose sodium	1.5
VI	Maltodextrin	6
10 VII	Pregelatinized starch	30
VIII	Croscarmellose sodium	15
IX	Purified water	51 + 15 + 15

The ingredients I and II were mixed in a beaker, wetted with 51 g water and then mixed  
 15 to a homogeneous mass. The ingredients III to VIII were added to a Moulinex laboratory  
 size mixer and mixed for 5 min, where to the homogeneous mass was added and mixed.  
 The beaker was rinsed with 2 x 15 g water and added to the mixer.

The extrudation and spheronizing procedure were performed as described in Example 1.  
 20

The release of lornoxicam from the pellet cores was determined by dissolution method II  
 (0.07 N HCl) and is as follows:

Time	Release (% w/w)
25 1h	5.7

Thus, only a very small amount of the lornoxicam present in the pellets is released at a  
 pH corresponding to that of 0.07 N HCl. The inclusion of an disintegrant such as, e.g.,  
 croscarmellose sodium does not seem to have any increasing effect on the release rate  
 30 of lornoxicam from the pellet cores. Furthermore, uncoated cores containing lornoxicam  
 do not seem to be a suitable choice in order to obtain a relatively fast release of  
 lornoxicam at low pH like the conditions in the stomach.

**EXAMPLE 7**

**Preparation of pellet cores – modification of the composition of the pellets in order to influence the release rate of lornoxicam**

5

Batch No. 19029836 (uncoated pellet cores) was prepared.

Lornoxicam pellet cores were prepared. The ingredients used are listed in Table 8.

10 Table 8

	Ingredients	Amount (g)
I	Lornoxicam	7.5
II	Sodium bicarbonate	37.7
15 III	Cellulose, microcrystalline	90.4
IV	Dibasic Calcium Phosphate, Anhydrous	104.1
V	Low-substituted Hydroxypropyl Cellulose	45.3
VI	Hydroxypropylcellulose	15
VII	Purified water	115.8
20 VIII	Ethanol 99.9 %	38.7

The ingredients II to IV were mixed in a Moulinex laboratory size mixer and mixed for 5 min. To 100 g of this mixture ingredient I was added and mixed in a cubus mixer for 5 min. The resulting mass was screened through a 0.5 mm screen and returned to the  
25 Moulinex mixer and mixed for further 6 min. A premixed mixture of ingredient VII and VIII was added to the powder mixture and massed for 6 min.

The resulting mass was then extruded and spheronized according to the method described in Example 1.

30

The release of lornoxicam from the pellet cores was determined by dissolution method II (0.07 N HCl) and is as follows:



Time	Release (% w/w)
After 1h	37.8

The release of lornoxicam from the pellets is significantly increased compared with the 5 pellets of Example 6, but still not quite satisfactory.

#### EXAMPLE 8

Preparation of pellets coated with a coating having varying amounts of a  
10 hydroxypropylmethylcellulose (HPMC)

Batch No. 23029833 (uncoated pellets) was prepared

Lornoxicam pellet cores were prepared as described in Example 4 and with the same  
15 composition.

The release of lornoxicam from the pellet cores was determined by dissolution method III (0.1 N HCl followed by pH 7.3) for 3 hours (i.e. 1 hour at a pH corresponding to the pH of 0.1 N HCl and 2 hours at pH 7.3) and is as follows:

20

Time	Release (% w/w)
10 min	36.9
1h	37.2
1 + 1 h:	86.4
25 1 + 2h:	95.7

Thus, the release in 0.1 N HCl is not very high (most of the lornoxicam which releases in 0.1 N HCl is released within the first 10 min) and the release rate is certainly not fast enough to anticipate that lornoxicam is released *in vivo* sufficiently fast to lead to a  
30 therapeutic effect.

In the following, two different batches of coated pellets of 100 g each were prepared.

Batch 1 (Batch No. 24029832 – coated pellet cores) :

35

100 g pellet cores were coated according to the procedure described in Example 1. The composition of the coating is as follows:

Ingredients	Amount (g)
<b>5 Inner coat</b>	
Hypromellose (Methocel E5 prem)	11.3
Magnesium stearate	0.6
Talc	5.4
Eudragit NE 30 D	191.7
10 Purified water	291
 <i>Outer coat</i>	
Hypromellose (method E% prem)	4.0
Talc	4.0
15 Purified water	96.0

The following amount of inner and outer coat was used:

Inner coat: 20.1 g coating solution (corresponding to a dry matter content of approximately 3% w/w of the pellet core weight; the HPMC content corresponds to 15.1% w/w).

Outer coat: 12.5 g coating solution (corresponding to a dry matter content of approximately 1% w/w of the pellet core weight).

**25 Batch 2 (Batch No.. 26029832 – coated pellet cores):**

100 g pellet cores were coated as described in Example 1. The composition of the coating is as follows:

Ingredients	Amount (g)
<i>Inner coat</i>	
Hypromellose (Methocel E5 prem.)	3.74
Magnesium stearate	0.17
35 Talc	1.48

65

Eudragit NE 30 D	31.9
Purified water	62.7

*Outer coat*

5 Hypromellose (method E% prem)	4.0
Talc	4.0
Purified water	96.0

The following amount of inner and outer coat was used:

10

Inner coat: 20.1 g coating solution (corresponding to a dry matter content of approximately 3% w/w of the pellet core weight; the HPMC content corresponds to 25% w/w).

Outer coat: 12.5 g coating solution (corresponding to a dry matter content of  
15 approximately 1% w/w of the pellet core weight).

**EXAMPLE 9****20 Preparation of a quick release granulate containing lornoxicam**

Batch No. 972510 (granulate) was prepared.

A granulate containing lornoxicam were prepared by using the ingredients listed in Table  
25 9. The composition of the granulate is essentially the same as that of the pellet cores of  
Example 7. The granulate was prepared in order to investigate whether it is possible to  
achieve a faster release of lornoxicam from a granulate than from pellet cores. From the  
results given below it is seen that the step of preparing pellets from a particulate  
composition containing lornoxicam has a dramatically decrease on the release rate of  
30 lornoxicam from the composition.

Table 9

	Ingredients	Amount (kg)
I	Lornoxicam	2.00
5 II	Sodium hydrogencarbonate	10.00
III	Cellulose microcristalline	24.00
IV	Calcium hydrogen phosphate anhydrous	27.60
V	Hydroxy Propyl Cellulose	4.00
VI	Low-Substituted Hydroxy Propyl Cellulose	12.00
10 VII	Purified water	27.00
VIII	Ethanol 96 %	9.00
IX	Calcium stearate	0.40

Ingredients II, III IV, V and VI were added to a Diosna intensive mixer and mixed for 1 min with the impeller speed I and chopper speed I. Out of this mixture, 10 kg was added the ingredient I by sieving through a Quadro Comil U20 with the sieve 062R in the following way: A part of the 10 kg mixture was sieved followed by ingredient I, whereafter the remaining of the 10 kg mixture was sieved. Ingredient I was not added to the mixture and mixed in the Diosna mixer for approximately 1 min.

20

A mixture of ingredient VII and VIII was added to the Diosna mixer, whereafter the granulation was started for 6 min with impeller speed I and with no use of the chopper.

After the granulation, the granulate was dried in a fluid bed until the outlet temperature had reached approximately 50°C and water content was below 1.0%, determined as LOD (Loss on Drying) when a sample of approximately 10 g was heated to a temperature of 70°C in 30 min. The granulate was sieved through a 0.71 sieve using a Frewitt siever. Oversized material was discarded.

30 Ingredient IX was sieved in the Quadro Comil with a sieve 062R and an equal amount of the granulate described above was added and mixed. This mixture was mixed with the remaining of the granulate in the Diosna mixer for 25 sec with an impeller speed of I and without using the chopper.

This mixture was compressed into a 9,5 mm concave tablets with a hardness of 80 to 100 N (the compression of the granulate was performed in order to avoid any of the problems which could arise during dissolution testing of a granulate and which are related to such bad wetting properties of a granulate that the granulate would float on the top of the dissolution medium giving rise to a *in vitro* unsatisfactory release of lornoxicam. However, later results have shown that granulates prepared in accordance with the above have suitable wetting properties, i.e. the final step of compression before dissolution testing is not necessary.

- 10 The dissolution of tablet cores was determined by the dissolution method II (0.07 N HCl) and is as follows:

Time	Release (% w/w)
20 min	100.6

15

The disintegration time of the tablets tested was at the most about 5 min. Thus, the dissolution rate of the granulate is expected to be of the same or quicker order of magnitude.

- 20 The release data given above are most surprising and give evidence that a fast release fraction containing a drug substance which is almost insoluble under acidic conditions can only be obtained if the composition is designed to a very fast release. In other words, application of traditionally prepared granulates and/or compositions made from such traditional granulates or particulate formulations do not seem to release the drug substance sufficiently fast under acidic conditions as those prevailing in the stomach. Accordingly, such traditional compositions are expected to release only a minor amount of the drug substance in the stomach and to release the remaining amount of lornoxicam in the intestines, i.e. after the composition reaches the intestines 1-3 hours after intake.

30

- Compared with the dissolution data given in Example 7 a dramatically increase in dissolution rate is observed for the granulate compared with the pellet cores. Thus, in order to achieve a very fast release of lornoxicam from a composition it seems as if the fast fraction advantageously may be constituted by a granulate rather than uncoated pellet cores or film-coated pellet cores.

**Conclusion with respect to Examples 1-9**

In the preceding examples it has been shown that pellets cores cannot release  
5 lornoxicam very quickly at pH 7,4 unless a surfactant is added (Examples 2 and 5), even  
though lornoxicam is soluble at pH 7,4. When a surfactant, e.g. polysorbate 20, was  
added the release at pH 7,4 was acceptable from the point of view that the core can  
enter an once daily formulations without significantly controlling the dissolution rate  
(Examples 1, 3 and 4). This control should ideally be taken care of by the applied  
10 lacquer.

When these pellet cores were analyzed with respect to dissolution behaviour under  
acidic conditions in which lornoxicam is only slightly soluble a satisfactory release was  
not obtained even if a surfactant was used (Examples 6 and 8). Therefore, another kind  
15 of subunits have to be used for the relatively fast releasing fraction. Subunits in the  
form of a granulate and with the composition as described in Example 9 seem to give a  
satisfactory fast release. However, subunits with the same formulation as in Example 9,  
but in the form of pellet cores, will not give a satisfactory release rate in acidic  
conditions as shown in Example 7.

20

**EXAMPLE 10****Preparation of a composition containing a mixture of uncoated and coated pellet cores**

25 The following example illustrate the dissolution behaviour of a composition containing a  
mixture of uncoated and coated pellet cores. The uncoated pellets are intended to  
simulate a fast release fraction and the coated pellets are intended to simulate a delayed  
release fraction.

30 Coated pellets obtained according to Example 1 were mixed with pellet cores obtained  
according to Example 4 and the final composition contained 40% of uncoated pellet  
cores and 60% coated pellets (the percentage is given as % w/w of the total dose of  
lornoxicam in the composition, i.e. the uncoated fraction accounts for 40% w/w of the  
total content of lornoxicam whereas the coated fraction accounts for 60% w/w of the

total content of lornoxicam. A unit dosage form of the composition contains 8 mg of lornoxicam.

The dissolution test was carried out according to dissolution method III. The following 5 dissolution data were obtained:

Time (h)	11029831 (uncoated fraction) + 05029833 (coated fraction) (5.5/4.3)* Release (% w/w)
0	0
0.5	1.4
1	2.9
2	38.4
3	46.1
4	49.6
5	53.5
6	55.9
7	59
8	61.4
9	64.6
10	67.2
11	69.2
13	74
14	75.6
15	77.9
16	79.3
17	80.7
18	82.5
19	83.6
20	85.3
21	86.4
22	87
23	88.1
24	89

\* (5.5/4.3) relates to the fact that the content of dry matter in the coat is 5.5% w/w and the HPML content is 4.3% w/w.



From the data given above it is seen that only 2.9% w/w lornoxicam is released after 1 hour. Thus, the "fast release fraction", i.e. the uncoated pellets, is not able to release all its content of lornoxicam under acidic conditions and during the first hour of the test. If this was the case, a release of about 40% is to be expected after 1 hour.

5

A dramatically increase in dissolution is observed after 2 hours reflecting the pH change of the dissolution medium 1 hour after the start of the test. Furthermore, a retardation of the release of lornoxicam is observed at pH 7.4 compared with the uncoated pellets cores, i.e. the coating is in control of the release rate. However, a composition

10 containing a mixture of uncoated and coated pellets does not seem to enable a fast release of lornoxicam. Therefore, the fast release fraction has to be manipulated in some way in order to release the active substance (lornoxicam) faster).

#### EXAMPLE 11

15

**Preparation of a composition containing a mixture of a quick release granulate and a delayed release fraction of coated pellet cores**

The composition described below was prepared in order to investigate the influence on  
20 the overall release rate of the granulate prepared in Example 9 which seems to have favourable properties with respect to a quick and very fast release of lornoxicam even under acidic conditions.

Coated pellets obtained according to Example 4 were mixed with a granulate obtained  
25 according to Example 9, where the mixture contained 40% w/w of the total dose of lornoxicam in the form of the granulate and the remaining 60% w/w of the total dose of lornoxicam was in the form of coated pellets (the concentration of lornoxicam in the granulate is about 2-3 % w/w and about 9% w/w in the uncoated pellets). The dissolution test was carried out according to dissolution method III. The following  
30 dissolution data was obtained:

72

Time (h)	972510 (granulate) + 20029832 (coated pellets) (3/4.3) Release (% w/w)
0	0
1	37.2
2	41.3
3	44.6
4	48.2
5	51.3
6	53.9
7	57
8	59.6
9	61.8
10	64.7
11	66.9
12	69.4
13	71.6
14	73.6
15	75.7
16	77.6
17	79.5
18	81.2
19	82.9
20	84.4
21	86
22	87.4
23	88.5
24	89.8

From the dissolution data given above, a fast release of lornoxicam is observed which is ascribed to the influence of the lornoxicam granulate.

In contrast to the results obtained in Example 10 a release of about 40% w/w of lornoxicam is observed after 1 hours. Thus, the above example gives evidence that a manipulation of the composition of the fast release fraction is necessary in order to achieve a suitable release even at a low pH. Furthermore, a delayed release is observed  
5 with respect to the coated pellets fraction.

## **EXAMPLE 12**

### **Investigation of the controlled release lacquer composition on the overall dissolution rate**

10

Coated pellets obtained according to Example 8 (batch 1, 15% w/w HPMC in the coat was mixed with granulate obtained according to Example 9. The mixture contained 40% w/w of the total dose of lornoxicam in the form of the granulate, whereas the remaining 60% w/w of lornoxicam was in the form of coated pellets. The dissolution test was  
15 carried out according to dissolution method III. The following dissolution data was obtained:

Time (h)	972510
	(granulate) + 24029832
	(coated pellets) (3/15.1)
	Release (% w/w)
0	0
0.5	35.7
1	35.7
2	43.2
3	50.0
4	55.8
5	60.9
6	66.2
7	70.7
8	74.4
9	78.3
10	81.5
11	84.8
12	87.3
13	89.3
14	91.1
15	92.6
16	93.8
17	95.0
18	95.9
19	96.6
20	97.2
21	97.5
22	97.8
23	98.0
24	97.5

From the dissolution data given above a much faster release of the delayed release fraction is observed compared with the results obtained in Example 11. Thus, the

composition of the coat can be adjusted to a suitable release rate. In this example the content of HPMC in the coat is 15.1% w/w.

### EXAMPLE 13

5

**Investigation of the influence of the composition of the controlled release coat on the release rate**

Coated pellets obtained according to Example 8 (batch 2) were mixed with a granulate  
10 obtained according to Example 9. The mixture contained 40% w/w of the lornoxicam content in the form of the granulate and the remaining 60% w/w in the form of coated pellets. The dissolution test was carried out according to dissolution method III.

The following dissolution data was obtained:

15

972510 (granulate) + 26029832	
Time (h)	(coated pellets) (3/25.0)
	Release (% w/w)
0	0
0.5	37.3
1	37.3
2	58
3	69.1
4	79.9
5	87.6
6	92.6
7	95.9
8	97.8
9	98.9
10	99.3
11	99.4
12	99.4
13	99.4
14	99.4
15	99.5

After 6 hours 92.6% w/w is released whereas only 69.4% w/w was released in Example 12. Thus, the increase of the concentration of HPMC in the coat (25% in the present example in contrast to 15% in Example 12) has an increasing effect on the release rate of lornoxicam from the composition.

#### **EXAMPLE 14**

##### **Determination of release rate of lornoxicam from controlled release pellets**

10

Dissolution data from coated pellets from Examples 1, 4 and 8 (batches 1 and 2) were determined by dissolution method I (pH 7.4). The following data have been obtained.

Time (h)	05029833 (coated pellets) (5.5/4.3) Example 1	20029832 (coated pellets) (3.0/4.3) Example 4	24029832 (coated pellets) (3.0/15.1) Example 8, batch 1	26029832 (coated pellets) (3.0/25.0) Example 8, batch 2
0	0	0	0	0
0.5	6.9	10.1	17.3	32.7
1	12.1	16.9	29	52.6
2	20.3	28.5	49.5	82.1
3	28.1	39.7	67.2	96.9
4	35.4	50	81.6	101.9
5	42	58.9	91.5	102.9
6	49.1	69.1	98.5	103
7	55.2	76.2	102.1	103.2
8	60.7	82.2	103.9	102.9
9	65.6	86.9	104.8	102.9
10	69.9	90.5	105.2	103.1
11	73.7	93.4	105.5	102.9
12	77.2	93.4	105.5	
13	80.3	95.2	105.8	
14	82.6	97.7	105.5	
15	85	97.9	105.8	
16	87.1	98	105.8	
17	88.6	98.7	105.9	
18	89.9	98.8	105.9	
19	91.2	99	105.8	

The data are also presented in Figure 3. Comparison of the results obtained from the composition of Example 1 with that of Example 4 illustrates that the thickness of the CR (controlled release) coat influences the release rate in such a manner that a thinner coat leads to a more rapid release. The influence of HPMC as an example of a substance which is capable of forming pores in the coat on the release rate is illustrated by the release rate of the two different batches of Example 8 and the results reveal an increasing release rate when the concentration of HPMC increases.

**Conclusion with respect to Examples 10-14**

In Examples 10-14, the preparation of a composition containing two fractions of  
5 subunits has been presented. One fraction representing a quick release part and the  
other fraction representing a controlled and delayed release part. Furthermore, the  
Examples illustrate the influence on the release rate of i) the composition of the quick  
release fraction and ii) composition and amount of lacquer applied on the controlled  
release fraction.

10

**EXAMPLE 15****Investigation of the influence of the dissolution medium on the release rate**

15 Dissolution data from coated pellets from Examples 4 and 8 (batch 2) were obtained  
using dissolution method V (pH 7.3), and are as follows:



Time (h)	20029832 (coated pellets) (3.0/4.3)[7.3] Example 4	26029832 (coated pellets) (3.0/25.0)[7.3] Example 8, batch 2
0	0	0
0.5	6.2	22
1	10.1	36.1
2	17.3	60.7
3	24.3	79.2
4	30.9	90.7
5	36.9	96.9
6	42.9	100.1
7	48.2	101.4
8	53.1	101.9
9	57.6	102
10	61.8	102
11	65.7	102
12	69.3	102
13	72.4	102
14	75.4	102
15	78	102
16	80.3	102
18	84.3	
20	87.3	

The data are compared with the data from Example 14 in Figure 3. An influence of the dissolution medium on the dissolution rate is observed, i.e. the choice of dissolution method is important (not only with respect to pH but also with respect to factors like, e.g., ionic strength, osmotic pressure etc.).

#### EXAMPLE 16

- Investigation of the influence of a pre-treatment in 0.1 N hydrochloric acid on the dissolution rate at pH 7.4

Dissolution data from coated pellets from Example 4 and Example 8 (batch 2) was determined by dissolution method I (pH 7.4) and method IV (1 hour at a pH corresponding to 0.1 N HCl and then at pH 7.4) and are as follows:

5

	26029832 (3,0/25)(HCl/7,4) Example 8, Time (h) batch 2	20029832 (3,0/4,3)(HCl/7,4) Example 4,	20029832 (3,0/4,3) Example 8 batch 2	26029832 (3,0/25,0) Example 4,
	in pH 7.4 Dissolution method IV	Dissolution method IV	Dissolution method I	Dissolution method I
0	0	0	0	0
0.5			10.1	32.7
1	47.6	16.9	16.9	52.6
2	77.5	29.1	28.5	82.1
3	92.4	39.6	39.7	96.9
4	98.1	48.3	50	101.9
5	100.2	56.9	58.9	102.9
6	100.6	64.8	69.1	103
7	100.6	71.6	76.2	103.2
8	100.7	77	82.2	102.9
9			86.9	102.9
10		85.7	90.5	103.1
11		88.8	93.4	102.9
12		91.3	93.4	
13		93.4	95.2	
14		94.8	97.7	
15		96	97.9	
16		97	98	
17		97.6	98.7	
18		98.3	98.8	
19		98.6	99	

The dissolution results from Example 16 reveal that a pre-treatment with acid does not have any significantly influence on the rate of release from the delayed release fraction, i.e. the coated pellets fraction.

- 5 In Figure 4 the data are presented and in order to make a proper comparison possible, the release data obtained by dissolution method IV have been displaced by 1 hour corresponding to the time period for treatment in 0.1 N HCl. Thus, in Figure 4, the zero setting for all compositions is when the dissolution medium has a pH of 7.4. The observed differences with respect to the dissolution of lornoxicam from Example 1 and  
10 4, respectively, are not significant and are within the standard deviation observed.

#### **Conclusion with respect to Examples 15 and 16**

The results from Examples 15 and 16 have shown that coated pellets have the same  
15 release rate independent on whether a pre-treatment in acid has been included or not whereas a change in the dissolution method (from method I to method V) has a significant influence on the release rate.

#### **EXAMPLE 17**

20

##### **Investigation on the influence of dose on the dissolution rate**

In this Example the dissolution profiles of a dose of 16 mg of lornoxicam are compared to a dose of 8 mg of lornoxicam. Dissolution profiles are obtained according to  
25 dissolution method III.

	972510 + 24029832	972510 + 24029832	972510 + 24029832
	8 mg	Reanalysis of	Reanalysis of
	Example 12	Example 12 (new	Example 12 (new
Time (h)	8 mg lornoxicam pr.	sample) 8 mg	sample) 16 mg
	capsule	lornoxicam pr.	lornoxicam pr.
		capsule	capsule
0	0	0	0
1	35.7	36.2	35.3
2	43.2	47	46.3
3	50.0	55.9	55
4	55.8	63.9	61.7
5	60.9	70.6	67.1
6	66.2	77.4	73.1
7	70.7	83	77.1
8	74.4	87.1	81.4
9	78.3	91.3	85.5
10	81.5	94.2	90.5
11	84.8	95.9	91.9
12	87.3	97.8	93.9
13	89.3	98.7	95.7
14	91.1	99	96.7
15	92.6	99.9	97.7
16	93.8	99.9	98.1
17	95.0	99.7	99
18	95.9	100.1	99.1
19	96.6		
20	97.2		
21	97.5		
22	97.8		
23	98.0		
24	97.5		

Data are presented in Figure 5 and the curves show that the dose is without any significant influence on the release rate. In Figure 5 a target profile calculated for

lornoxicam has been included and it is seen that the compositions tested have profiles very close to the target profile.

#### EXAMPLE 18

5

##### Investigation on whether a plain granulate quickly releases an NSAID substance

A granulate containing naproxen was prepared using the ingredients listed in Table 10. The granulate was prepared in order to investigate whether a plain granulate like the one disclosed in EP-A-0 438 249A1 (ELAN Corporation P.L.C.) releases naproxen quickly (as defined herein) when the dissolution testing is done according to dissolution method II (n = 2) described herein. No standards were used and, accordingly, a literature value for E (1%, 1 cm) = 63 was used to calculate the content in the samples. The composition of the granulate corresponds to the one disclosed in Example 1 of EP-A-0 438 249A1  
15 (ELAN Corporation P.L.C.).

Table 10

Ingredients	Amount (g)
20 Naproxen	232.0
Polyvidone 30	7.2
Isopropanol	65.7

25 Naproxen and polyvidone 30 were mixed in a lab scale Kenwood mixer for 3 min. The mixture was granulated by slowly adding the isopropanol over a period of 2 min and the mixing was continued for 1 min. Then the granulate was dried on trays at 50 °C for 12 hours. Thereafter half of the granulate was sieved through a 500 µm sieve and the other half of the granulate was sieved through a 1000 µm sieve. Oversized material was  
30 discarded in both cases. The thus obtained two granulates were tested according to dissolution method II described herein.

Batch No. 26089831: 500 µm sieved granulate in an amount corresponding to a 150 mg tablet. In the following is given the results from the dissolution test.

35

84

Time (h)	Release (dissolved naproxen) % w/w
0	0
5 0.5	15
1	16.1
1.5	16.5
2	17.6

- 10 Batch No. 26089831: 1000  $\mu$ m sieved granulate in an amount corresponding to a 150 mg tablet. In the following is given the results from the dissolution test.

Time (h)	Release (dissolved naproxen) % w/w
15 0	0
0.5	11.4
1	13.4
1.5	14.2
20 2	15.7

From the results given above, it is clear that such plain formulations do not release the NSAID substance very fast and, accordingly, such formulations or compositions do not fall under the definition of quick release defined herein (i.e. that at least about 50% of the NSAID substance is released within the first 20 min of the dissolution test).

**CLAIMS**

1. An oral pharmaceutical modified release multiple-units composition in unit dosage form for administration of a therapeutically and/or prophylactically effective amount of a non-steroid anti-inflammatory drug substance (an NSAID substance), a unit dosage form comprising at least two NSAID-containing fractions,

i) a first NSAID-containing fraction of multiple-units for quick release of the NSAID substance, and

10

ii) a second NSAID-containing fraction of multiple-units for extended release of the NSAID substance,

the first fraction which - when subjected to dissolution method II as defined herein employing 0.07 N HCl as dissolution medium - releases at least 50% w/w of the NSAID substance present in the fraction within the first 20 min of the test,

the second fraction being in the form of coated delayed release multiple units for extended release of the NSAID substance.

20

2. A composition according to claim 1, wherein the first fraction - when subjected to dissolution method II as defined herein employing 0.07 N HCl as dissolution medium - releases at least 55% w/w such as, e.g., at least about 60% w/w, at least about 65% w/w, at least about 70% w/w, at least about 75% w/w or at least about 80% w/w of the total NSAID substance present in the first fraction within the first 20 min of the test.

25

3. A composition according to claim 1 or 2, wherein the quick *in vitro* release and the extended *in vitro* release being adapted so that the first fraction is substantially released when the release from the second fraction is initiated corresponding to at least 50% w/w release of the NSAID substance contained in the first fraction at the time when at the most 15% w/w such as at the most 10% w/w or at the most 5% w/w of the NSAID substance contained in the second fraction is released as measured by the dissolution method III defined herein.

35

4. A composition according to any one of the preceding claims, wherein the NSAID substance contained in the first fraction has a  $pK_a$  value between from about 3.0 to about 5.5 and the first fraction is in the form of uncoated units.
- 5 5. A composition according to any one of the preceding claims, wherein the NSAID substance has a solubility in 0.1 N hydrochloric acid at room temperature of at the most about 0.5% w/v such as, e.g. at the most about 0.1% w/v, at the most about 0.05% w/v, at the most about 0.03% w/v, at the most about 0.01% w/w, at the most about 0.007% w/v, at the most about 0.005% w/v, at the most about 0.003% w/v, at the  
10 most about 0.002% w/v or at the most about 0.001% w/v.
6. A composition according to any one of claims 1-3, wherein the NSAID substance contained in the first fraction has a  $pK_a$  value of at least 5.0 such as at least about 5.5.
- 15 7. A composition according to claim 6, wherein the first fraction is present in the form of coated units.
8. A composition according to any one of claims 1-3 or 6-7, wherein the NSAID substance has a solubility in 0.1 N hydrochloric acid at room temperature of at least  
20 about 0.1% w/v such as e.g. at least about 0.5% w/v or at least about 1% w/v.
9. A composition according to any one of the preceding claims intended for administration once or twice daily.
- 25 10. A composition according to any one of the preceding claims for the administration of a therapeutically and/or prophylactically effective amount of an NSAID substance to obtain both a relatively fast onset of the therapeutic effect and the maintenance of therapeutically active plasma concentration for a relatively long period of time, a unit dosage of the composition comprising at least two fractions as follows:  
30
- a first fraction of quick release multiple-units for relatively quick release *in vivo* of an NSAID substance to obtain a therapeutically and/or prophylactically active plasma concentration within a relatively short period of time, and



a second fraction of coated modified release multiple-units for extended release *in vivo* of an NSAID substance to maintain a therapeutically and/or prophylactically active plasma concentration in order to enable dosing once or twice daily,

- 5 the formulation of the first and the second fractions, with respect to release therefrom and with respect to the ratio between the first and the second fraction in the unit dosage, being adapted so as to obtain:

a relative quick *in vitro* release of the NSAID substance from the first fraction of quick  
10 release multiple-units, as measured by the dissolution method II as defined herein,

an extended *in vitro* release of the NSAID substance from the second fraction of extended release multiple-units relative to the *in vitro* release of the first fraction of the NSAID substance, as measured by e.g. the dissolution method III as defined herein,

15

the quick release and the extended *in vitro* release being adapted so that the first fraction is substantially released when the release from the second fraction is initiated corresponding to at least 50% w/w release of the NSAID substance contained in the first fraction at the time when at least about 15% w/w such as, e.g., at least about  
20 10% w/w or at least about 5% w/w of the NSAID substance contained in the second fraction is released as measured by the dissolution method III defined herein.

11. A composition according to any one of the preceding claims, wherein the NSAID substance is selected from the group consisting of lornoxicam, diclofenac, nimesulide,  
25 ibuprofen, piroxicam, piroxicam (betacyclodextrin), naproxen, ketoprofen, tenoxicam, aceclofenac, indometacin, nabumetone, acemetacin, morniflumate, meloxicam, flurbiprofen, tiaprofenic acid, proglumetacin, mefenamic acid, fenbufen, etodolac, tolfenamic acid, sulindac, phenylbutazone, fenoprofen, tolmetin, acetylsalicylic acid, dexibuprofen, and pharmaceutically acceptable salts, complexes and/or prodrugs thereof  
30 and mixtures thereof.

12. A composition according to any one of the preceding claims, wherein the NSAID substance in the first fraction is the same as the NSAID substance contained in the second fraction.

35

13. A composition according to any one claims 1-11, wherein the NSAID substance in the first fraction is different from the NSAID substance contained in the second fraction.
14. A composition according to any one of the preceding claims, wherein the NSAID substance in the first fraction is lornoxicam.
15. A composition according to any one of the preceding claims, wherein the NSAID substance in the second fraction is lornoxicam.
16. A composition according to any one of the preceding claims comprising a further active drug substance.
17. A composition according to any one of the preceding claims, wherein a further active drug substance is included in at least one of the first and second fraction.
18. A composition according to claim 16 or 17, wherein the further active drug substance is an antidepressant, an opioid, a prostaglandine analog (e.g. misoprostol), a glucocorticosteroid, a cytostaticum (e.g. methotrexate), a H<sub>2</sub> receptor antagonist (e.g. cimetidine, ranitidine), a proton pump inhibitor (e.g. pantoprazole, omeprazole, lansoprazole) and/or an antacidum.
19. A composition according to claim 16 or 17, wherein the further active drug substance is paracetamol, penicillamine, sulfasalazine and/or auranorfin.
20. A composition according to any one of the preceding claims, wherein the NSAID substance is lornoxicam.
21. A composition according to any one of the preceding claims, wherein the quick release multiple-units of the first fraction have a mean particle size of at the most about 250 µm such as, e.g. at the most about 240 µm, at the most about 230 µm, at the most about 220 µm, at the most about 210 µm, at the most about 200 µm, at the most about 190 µm, at the most about 180 µm, at the most about 175 µm, at the most about 150 µm, at the most about 125 µm, at the most about 100 µm, at the most about 90 µm or at the most about 80 µm.

22. A composition according to any one of the preceding claims, wherein the *in vitro* dissolution characteristics of the first fraction of quick release multiple-units provides within 1 hour a release as defined by the dissolution method II defined herein of at least 50% w/w, such as, e.g., at least about 60% w/w, at least about 70% w/w, at at least  
5 about 80% w/w, at least about 85% w/w at least about 90% w/w or at least about 95% w/w of the NSAID substance.

23. A composition according to any one of the preceding claims, wherein the *in vitro* dissolution characteristics of the second fraction of extended release multiple-units  
10 provides within 1 hour a release as defined by the dissolution method III defined herein in the range of 0%-30% w/w, such as in the range of 0%-20% w/w, in the range of 0%-10% w/w, such as at the most about 5% w/w of the NSAID substance.

24. A composition according to any one of the preceding claims, wherein the *in vitro* dissolution characteristics of the second fraction of extended release multiple-units  
15 provides within 3 hours a release as defined by the dissolution method III defined herein in the range of about 10%-70% w/w, such as, e.g., in the range of about 10%-60% w/w, in the range of about 12%-50% w/w, in the range of 14%-45% w/w, in the range of about 15%-30% w/w, in the range of about 15%-20% w/w such as, e.g., about  
20 17% w/w of the NSAID substance.

25. A composition according to any one of the preceding claims, wherein the *in vitro* dissolution characteristics of the second fraction of extended release multiple-units provides within 6 hours a release as defined by the dissolution method III defined herein  
25 in the range of about 35%-95% w/w, such as, e.g., in the range of about 50%-90% w/w, in the range of about 50%-80% w/w, in the range of 50%-75% w/w, in the range of about 50%-60% w/w, in the range of about 53%-59% w/w such as, e.g. about 56% w/w of the NSAID substance.

30 26. A composition according to any one of the preceding claims, wherein the *in vitro* dissolution characteristics of the second fraction of modified release multiple-units provides within 9 hours a release as defined by the dissolution method III defined herein in the range of about 50%-100% w/w, such as, e.g., in the range of about 60%-98% w/w, in the range of about 65%-95% w/w, in the range of about 70%-90% w/w, in the  
35 range of about 70%-80% w/w such as, e.g., about 76% w/w of the NSAID substance.

27. A composition according to any one of the preceding claims, wherein the *in vitro* dissolution characteristics of the first and second fractions are adapted so that the first fraction is substantially released when the release from the second fraction is initiated  
5 corresponding to at least 50% w/w of the first fraction at the time at the most about 15% w/w such as, e.g., at the most about 10% w/w or at the most about 5% w/w of the second fraction is released as measured by the dissolution method III defined herein.

28. A composition according to any one of the preceding claims, wherein the *in vitro*  
10 dissolution characteristics of the first and second fractions are adapted so that the first fraction is substantially released when the release from the second fraction is initiated corresponding to at least 70% w/w release of the first fraction at the time at the most about 20% w/w such as, e.g. at the most about 15% or at the most about 10% w/w of the second fraction is released as measured by the dissolution method III as defined  
15 herein.

29. A composition according to any one of the preceding claims, wherein the *in vitro* dissolution characteristics of the composition provides within 1 hour a release of the NSAID substance from the composition in the range of about 5-50% w/w, such as,  
20 e.g., in the range of about 5-45% w/w, in the range of about 15-40% w/w, in the range of about 20-35% w/w such as about 29% w/w, as defined by the dissolution method III as defined herein.

30. A composition according to any one of the preceding claims, wherein the *in vitro*  
25 dissolution characteristics of the composition provides within 3 hours a release as defined by the dissolution method III as defined herein in the range of about 20-80% w/w, such as, e.g., in the range of about 25-70% w/w, in the range of about 30-60% w/w, in the range of about 35-55% w/w such as about 42% w/w.

30 31. A composition according to any one of the preceding claims, wherein the *in vitro* dissolution characteristics of the composition provides within 6 hours a release as defined by the dissolution method III defined herein in the range of about 40-98% w/w, such as, e.g., in the range of about 50-95% w/w, in the range of about 60-90% w/w, in the range of about 60-85% w/w, most preferred in the range of about 60-83% w/w  
35 such as about 69% w/w.

32. A composition according to any one of the preceding claims, wherein the *in vitro* dissolution characteristics of the composition provides within 9 hours a release as defined by the dissolution method III as defined herein in the range of about 50-100%  
5 w/w, such as, e.g., in the range of about 60-99% w/w, in the range of about 70-98% w/w, in the range of about 70-97% w/w, in the range of about 75-96% w/w, in the range of about 80-96% w/w, about 80-85% w/w such as about 83% w/w.

33. A composition according to any one of the preceding claims, wherein the  
10 percentage of NSAID substance in the first fraction is in the range of about 5%-50% w/w such as, e.g., in the range of about 10%-45% w/w, in the range of about 15%-45% w/w, in the range of about 20%-40% w/w, in the range of about 25%-40% w/w, in the range of about 25%-35% w/w such as, e.g., about 30% w/w, calculated on the total amount of NSAID substance in the composition.

15

34. A composition according to any one of the preceding claims, wherein the percentage of NSAID substance in the second fraction is in the range of about 30%-99% w/w such as, e.g. in the range of about 40%-98% w/w, in the range of about 45%-95% w/w, in the range of about 50%-95% w/w, in the range of about 55%-85%  
20 w/w, in the range of about 60%-80% w/w, in the range of about 60%-75% w/w, in the range of about 65%-75% w/w such as, e.g., about 70% w/w, calculated on the total amount of NSAID substance in the composition.

35. A composition according to any one of the preceding claims, wherein the multiple-  
25 units of the second fraction are coated cross-sectionally substantially homogeneous pellets.

36. A composition according to any one of the preceding claims, wherein the multiple-units of the first fraction are cross-sectionally substantially homogeneous pellets.

30

37. A composition according to any one of the preceding claims, wherein the first fraction results in a peak plasma concentration of NSAID substance which is substantially the same as the peak plasma concentration resulting from the second fraction.

35

38. A composition according to any one of claims 1-36, wherein the first fraction results in a peak plasma concentration of the NSAID substance which is higher than the peak plasma concentration resulting from the second fraction.

5 39. A composition according to any one of claims 1-36, wherein the first fraction results in a peak plasma concentration of the NSAID substance which is lower than the peak plasma concentration resulting from the second fraction.

40. A composition according to any one of the preceding claims, wherein the first  
10 fraction results in a therapeutically active plasma concentration of the NSAID substance until the extended release of an NSAID substance from the second fraction of modified release multiple-units contributes to the maintenance of a therapeutically active plasma concentration of the NSAID substance.

15 41. A composition according to any one of the preceding claims, wherein the extended release coating of the second fraction is substantially water-insoluble, but water-diffusible and substantially pH-independent.

42. A composition according to any one of the preceding claims, wherein the first  
20 fraction is coated units and the coating is a substantially water-insoluble, but water-diffusible and substantially pH-independent coating.

43. A composition according to any one of the preceding claims, wherein a unit dosage of the composition comprises from about 1 to about 32 mg of the NSAID substance.  
25

44. A composition according to any one of claims 1-42, wherein a unit dosage comprises from about 1 mg to about 1.6 g such as from about 1 mg to about 1.2 g of the NSAID substance.

30 45. A composition according to any one of claims 1-42, wherein a unit dosage comprises from about 50 mg to about 1.1 g of the NSAID substance.

46. A composition according to any one of claims 1-42, wherein a unit dosage comprises from about 100 mg to about 1.0 g of the NSAID substance.

47. A composition according to any one of claims 1-42, wherein a unit dosage comprises from about 200 mg to about 900 mg of the NSAID substance.

48. A composition according to any one of claims 1-42, wherein a unit dosage  
5 comprises from about 300 mg to about 800 mg of the NSAID substance.

49. A composition according to any one of the preceding claims comprising a unit dosage for the administration of the therapeutically effective amount of the NSAID substance twice daily.

10

50. A composition according to any one of claims 1-48 comprising a unit dosage for the administration of the therapeutically effective amount of the NSAID substance once daily.

15 51. A composition according to any one of the preceding claims wherein the unit dosage of the composition is in the form of a capsule, tablet or sachet.

52. A composition according to any one of the preceding claims, wherein the NSAID substance is lornoxicam and the unit dosage of the composition contains 4, 8, 12, 16,  
20 20, 24, 28, 32 or 36 mg of lornoxicam.

53. A process for the preparation of a unit dosage form of an oral pharmaceutical modified release composition according to any one of the preceding claims, the process comprising incorporating into the unit dosage form at least two fractions as follows:  
25 a first fraction of quick release multiple-units for relatively quick release *in vivo* of an NSAID substance to obtain a therapeutically or prophylactically active plasma concentration within a relatively short period of time, and a second fraction of coated extended release multiple-units for extended release *in vivo* of an NSAID substance to maintain a therapeutically active plasma concentration in order to enable dosing once or  
30 twice daily,

the formulation of the first and the second fractions, with respect to release therefrom and with respect to the ratio between the first and the second fraction in the unit dosage, being adapted so as to obtain:

35

a relative quick *in vitro* release of the NSAID substance from the first fraction of quick release multiple-units, as measured by the dissolution method II defined herein,

an extended *in vitro* release of the NSAID substance from the second fraction of

- 5 extended release multiple-units relative to the *in vitro* release of the first fraction of the NSAID substance, as measured by the dissolution method III as defined herein, the quick release and the extended *in vitro* release being adapted so that the first fraction is substantially released when the release from the second fraction is initiated corresponding to at least about 50% w/w release of the NSAID substance contained in
- 10 the first fraction at the time when at the most about 15% w/w such as, e.g., at the most about 10% w/w or at the most about 5% w/w of the NSAID substance contained in the second fraction is released as measured by the dissolution method III as defined herein.

- 15 54. A method for treating a patient suffering from pain and/or inflammatory conditions and/or the like comprising administering to the patient an effective amount of an NSAID substance in the form of a composition according to any one of claims 1-52 once or twice daily.
- 20 55. A method for administering a therapeutically and/or prophylactically effective amount of an NSAID substance to a patient in need thereof to obtain both a relatively fast onset of the therapeutic effect and the maintenance of therapeutically active plasma concentration for a relatively long period of time, the method comprising administering once or twice daily a unit dosage of a composition comprising at least two
- 25 fractions as follows:

a first fraction of quick release multiple-units for relatively quick release *in vivo* of an NSAID substance to obtain a therapeutically and/or prophylactically active plasma concentration within a relatively short period of time, and

30

a second fraction of coated modified release multiple-units for extended release *in vivo* of an NSAID substance to maintain a therapeutically and/or prophylactically active plasma concentration.

35



1/5

# NSAID plasma concentrations Normalised to same dose

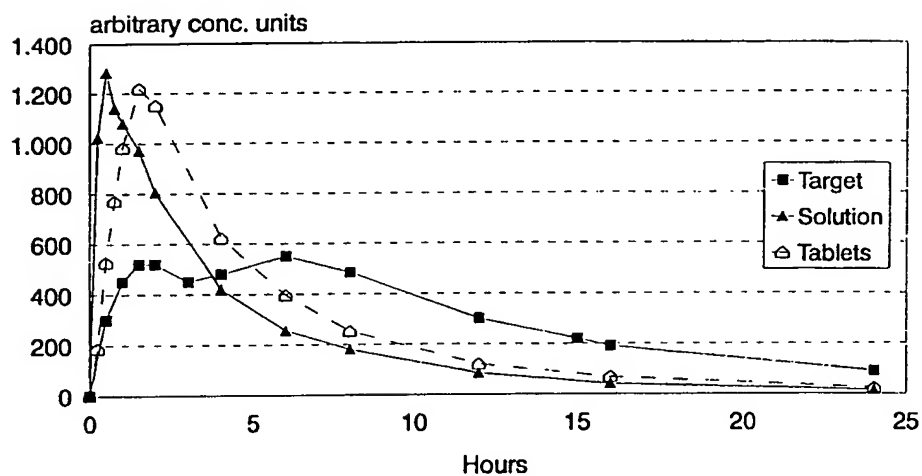
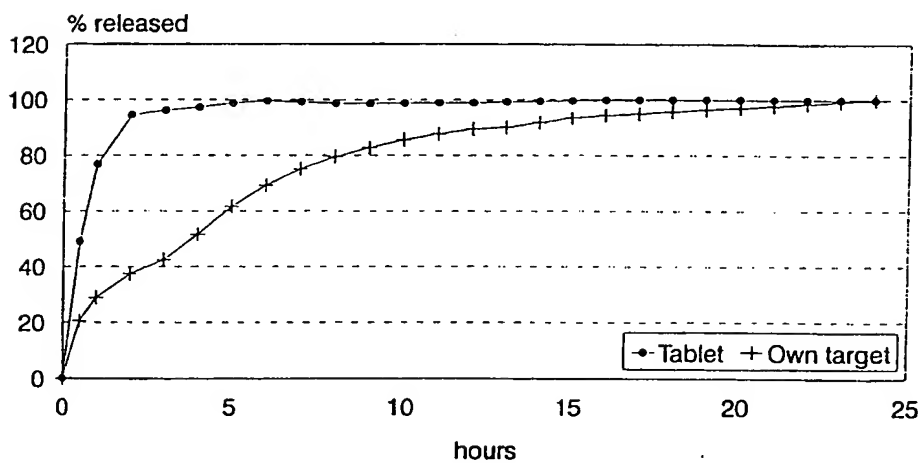


Fig. 1

2/5

## Lornoxicam in vivo dissolution based on deconvolution

**Fig. 2**

3/5

Lornoxicam dissolution, 8 mg

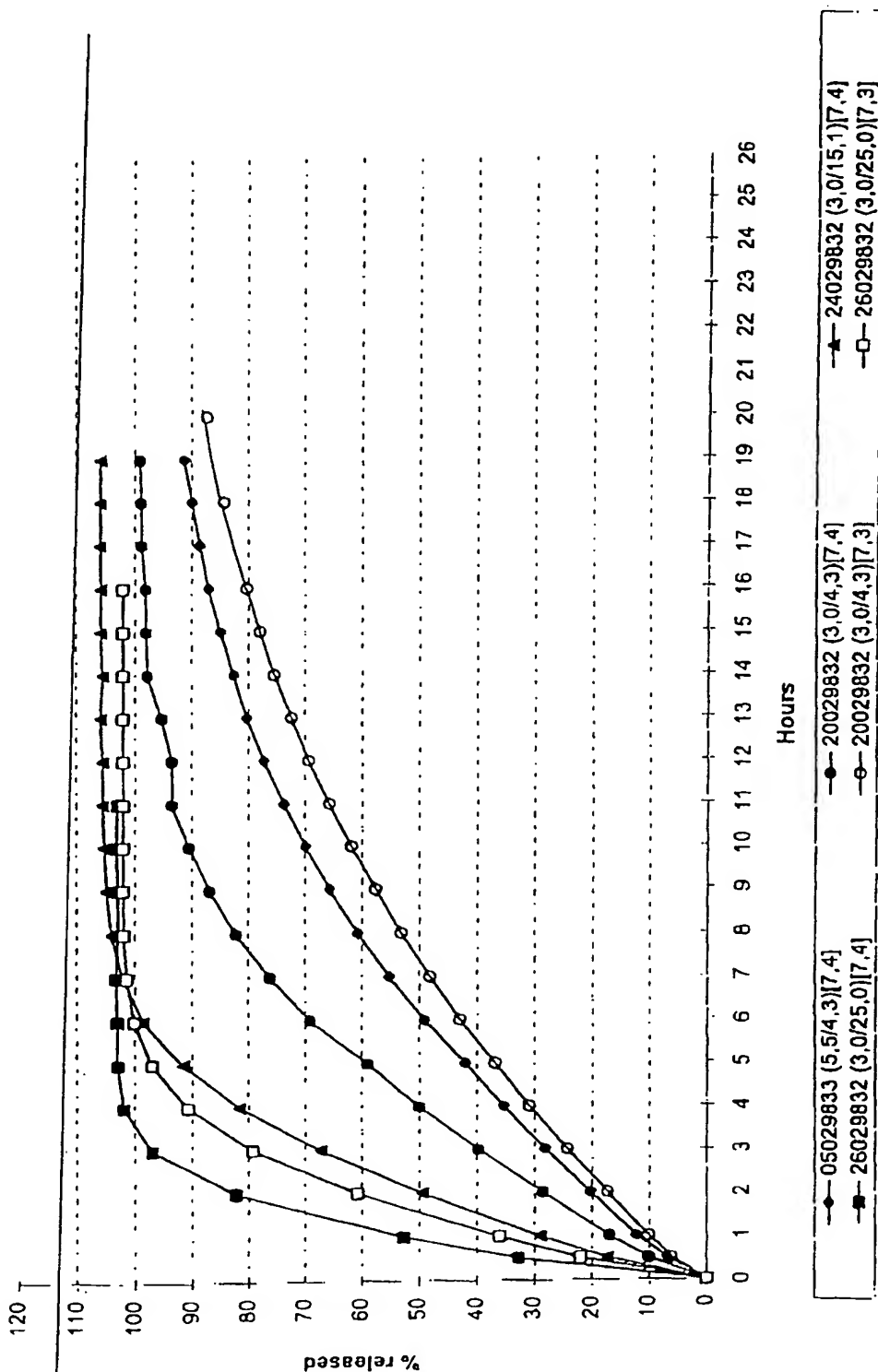


Fig. 3

4/5

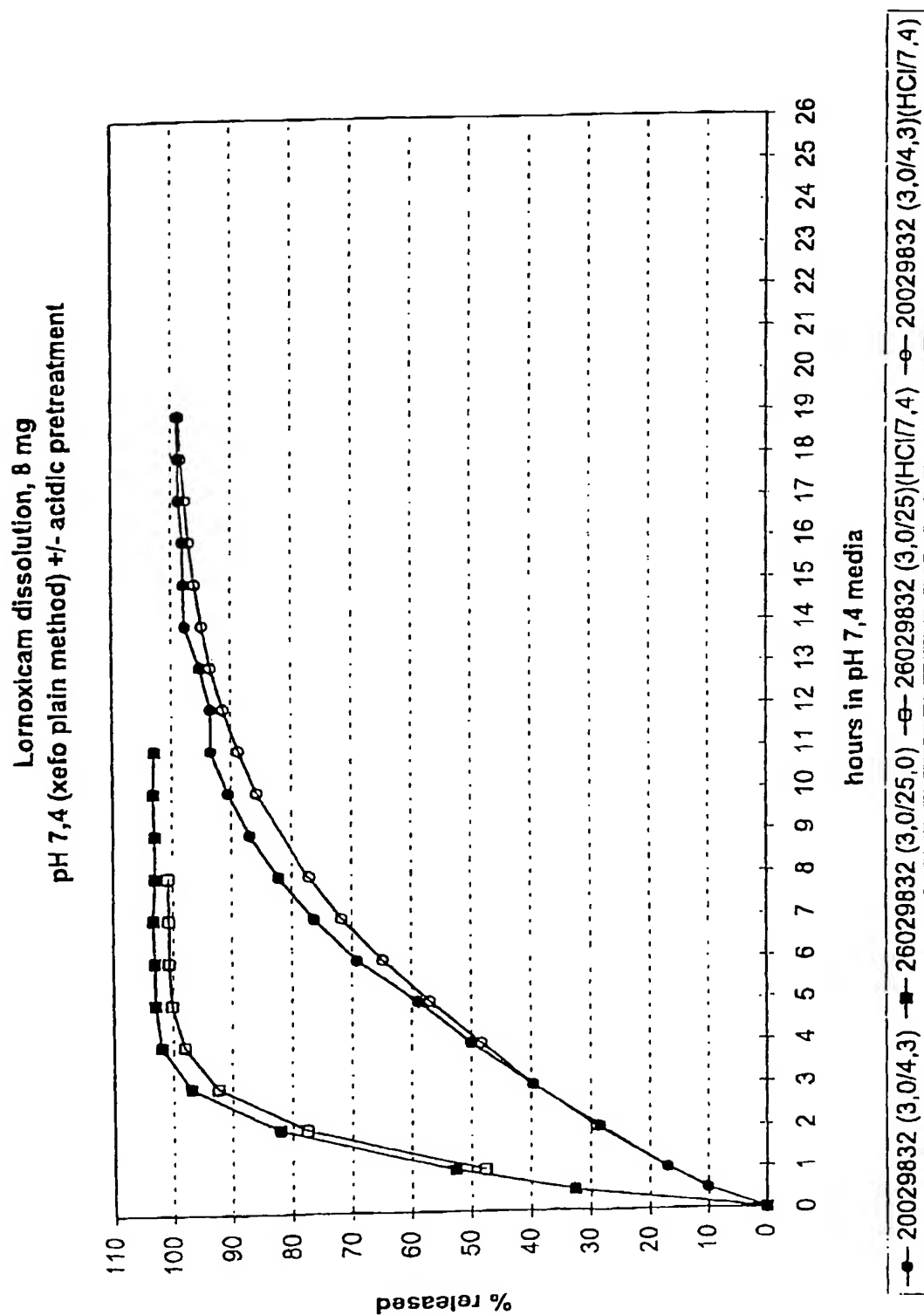


Fig. 4

5/5

Lornoxicam dissolution, 8/16 mg dose  
0,1 N HCl 1h, then pH 7,3

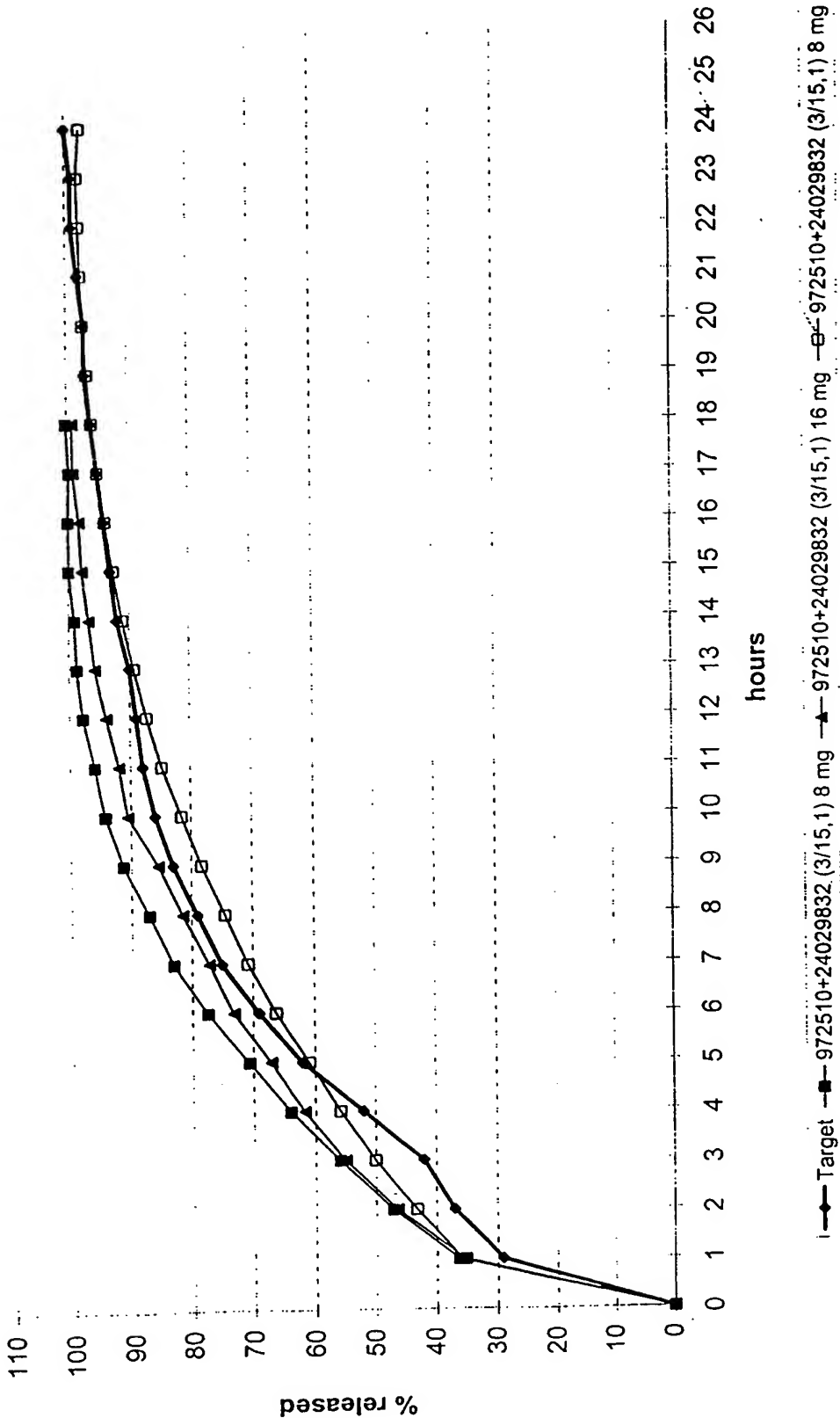


Fig. 5

# INTERNATIONAL SEARCH REPORT

International Application No

PCT/DK 98/00388

A. CLASSIFICATION OF SUBJECT MATTER  
IPC 6 A61K9/20 A61K9/50 A61K31/00

According to International Patent Classification (IPC) or to both national classification and IPC

## B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

IPC 6 A61K

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)

## C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X,Y	US 5 043 167 A (ROTINI LEONE G ET AL) 27 August 1991	1-13, 16-19, 21-51, 53,54
Y	see the whole document	14,15, 20,52
X,Y	EP 0 438 249 A (ELAN CORP PLC) 24 July 1991	1-13, 16-19, 21-51, 53,54
	see the whole document	
Y	US 5 478 577 A (SACKLER RICHARD ET AL) 26 December 1995 see the whole document	1-13
	--- -/--	

☒ Further documents are listed in the continuation of box C.

☒ Patent family members are listed in annex.

### \* Special categories of cited documents :

- \*"A" document defining the general state of the art which is not considered to be of particular relevance
- \*"E" earlier document but published on or after the international filing date
- \*"L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)
- \*"O" document referring to an oral disclosure, use, exhibition or other means
- \*"P" document published prior to the international filing date but later than the priority date claimed

\*"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention

\*"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone

\*"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art.

\*"&" document member of the same patent family

Date of the actual completion of the international search

8 December 1998

Date of mailing of the international search report

21/12/1998

Name and mailing address of the ISA

European Patent Office, P.B. 5818 Patentlaan 2  
NL - 2280 HV Rijswijk  
Tel. (+31-70) 340-2040, Tx. 31 651 epo nl,  
Fax: (+31-70) 340-3016

Authorized officer

Fischer, W

# INTERNATIONAL SEARCH REPORT

Inter national Application No

PCT/DK 98/00388

## C.(Continuation) DOCUMENTS CONSIDERED TO BE RELEVANT

Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
Y	WO 97 06787 A (DYER ALISON MARGARET ;CSIR (ZA); ROLFES HEIDI (ZA); MERWE THILO LO) 27 February 1997 see abstract see page 5, line 25-29 see page 14, line 1 - line 4 ---	14, 15, 20, 52
P, X, Y	WO 97 32573 A (NYCOMED DANMARK A S ;SKINHOEJ ANETTE (DK)) 12 September 1997	1-13, 16-19, 21-51, 53, 54
L	"L": DOCUMENT SO QUOTED SINCE IT CASTS DOUBT ON THE VALIDITY OF THE CONVENTION-PRIORITY CLAIMED see the whole document -----	

# INTERNATIONAL SEARCH REPORT

International application No.

PCT/DK 98/00388

## Box I Observations where certain claims were found unsearchable (Continuation of item 1 of first sheet)

This International Search Report has not been established in respect of certain claims under Article 17(2)(a) for the following reasons:

1. ☒ Claims Nos.: 54  
because they relate to subject matter not required to be searched by this Authority, namely:  
Remark: Although claim(s) 54  
is(are) directed to a method of treatment of the human/animal  
body, the search has been carried out and based on the alleged  
effects of the compound/composition.
2. ☐ Claims Nos.:  
because they relate to parts of the International Application that do not comply with the prescribed requirements to such  
an extent that no meaningful International Search can be carried out, specifically:
3. ☐ Claims Nos.:  
because they are dependent claims and are not drafted in accordance with the second and third sentences of Rule 6.4(a).

## Box II Observations where unity of invention is lacking (Continuation of item 2 of first sheet)

This International Searching Authority found multiple inventions in this international application, as follows:

1. ☐ As all required additional search fees were timely paid by the applicant, this International Search Report covers all  
searchable claims.
2. ☐ As all searchable claims could be searched without effort justifying an additional fee, this Authority did not invite payment  
of any additional fee.
3. ☐ As only some of the required additional search fees were timely paid by the applicant, this International Search Report  
covers only those claims for which fees were paid, specifically claims Nos.:
4. ☐ No required additional search fees were timely paid by the applicant. Consequently, this International Search Report is  
restricted to the invention first mentioned in the claims; it is covered by claims Nos.:

Remark on Protest

- ☐ The additional search fees were accompanied by the applicant's protest.
- ☐ No protest accompanied the payment of additional search fees.



FURTHER INFORMATION CONTINUED FROM PCT/ISA/ 210

Although claims 54 is directed to a method of treatment of the human/animal body, the search has been carried out and based on the alleged effects of the compound/composition.

-----

Claims Nos.: 54

Rule 39.1(iv) PCT - Method for treatment of the human or animal body by therapy

# INTERNATIONAL SEARCH REPORT

information on patent family members

Inter. nat Application No

PCT/DK 98/00388

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
US 5043167 A	27-08-1991	AU 2766689 A	20-07-1989
		DE 3879166 A	15-04-1993
		DK 18089 A	19-07-1989
		EP 0324981 A	26-07-1989
		ES 2053702 T	01-08-1994
		FI 890238 A	19-07-1989
		GR 3007312 T	30-07-1993
		JP 1279823 A	10-11-1989
		PT 89467 A,B	08-02-1990
EP 0438249 A	24-07-1991	IE 66933 B	07-02-1996
		AT 126055 T	15-08-1995
		AU 639519 B	29-07-1993
		AU 6933291 A	18-07-1991
		CA 2034096 A	16-07-1991
		DE 69111832 D	14-09-1995
		DE 69111832 T	14-03-1996
		DK 438249 T	18-09-1995
		ES 2075338 T	01-10-1995
		GR 3017633 T	31-01-1996
		IL 96900 A	31-12-1995
		JP 4217918 A	07-08-1992
		US 5637320 A	10-06-1997
US 5478577 A	26-12-1995	AU 693134 B	25-06-1998
		AU 1331395 A	13-06-1995
		BG 100346 A	31-07-1996
		CN 1130352 A	04-09-1996
		CZ 9503217 A	17-07-1996
		EP 0731694 A	18-09-1996
		FI 955782 A	30-01-1996
		HU 73976 A	28-10-1996
		JP 9505602 T	03-06-1997
		NO 954925 A	23-05-1996
		NZ 277917 A	27-04-1998
		NZ 329909 A	27-04-1998
		PL 312587 A	29-04-1996
		SK 153895 A	05-06-1996
		WO 9514460 A	01-06-1995
		US 5672360 A	30-09-1997
WO 9706787 A	27-02-1997	AU 6824996 A	12-03-1997
		CA 2228610 A	27-02-1997
		EP 0844870 A	03-06-1998
WO 9732573 A	12-09-1997	AU 2021997 A	22-09-1997